

Super-Resolution Imaging of Voltages in the Interior of Individual, Vital Mitochondria

ChiaHung Lee, Douglas C. Wallace, and Peter J. Burke*



pharmacological manipulation. Changes in mitochondrial membrane potential as a function of time and position can be imaged in different metabolic states (not possible in whole cells), created by the addition of substrates and inhibitors of the electron transport chain, enabled by the isolation of vital mitochondria. By careful analysis of structure dyes and voltage dyes (lipophilic cations), we demonstrate that most of the fluorescent signal seen from voltage dyes is due to membrane bound dyes, and develop a model for the membrane potential dependence of the fluorescence contrast for the case of super-



resolution imaging, and how it relates to membrane potential. This permits direct analysis of mitochondrial structure and function (voltage) of isolated, individual mitochondria as well as submitochondrial structures in the functional, intact state, a major advance in super-resolution studies of living organelles.

KEYWORDS: Voltage, mitochondria, super-resolution, fluorescent dye, metabolism, electrophysiology, lipid bilayer

nalysis of mitochondrial structure and function is increasingly being recognized as central to under-Lstanding human health and disease.¹⁻⁶ Yet mitochondria within tissue cells can have markedly different structures and functions. Hence, there is a critical need to be able to characterize the structure and function of the individual isolated mitochondrion. One of the most important mitochondrial functions is the generation of cellular ATP by oxidative phosphorylation (OXPHOS). OXPHOS consists of the electron transport chain (ETC) plus the ATP synthase. The four multisubunit enzyme complexes of the mitochondrial inner membrane ETC (complexes I-IV) oxidize hydrogen derived from carbohydrates and fats with oxygen to generate H₂O. Starting with NADH for complex I or succinate for complex II, the electrons are transferred to coenzyme Q₄ then complex III, through cytochrome c to complex IV, and then on to oxygen. As the electrons transverse complex I, III, and IV, protons derived from $H_2O(H^+ + OH^-)$ are transported out of the mitochondrial matrix to create an electrochemical gradient that is negative and alkali in the matrix and positive and acidic on the opposite side of the inner membrane. Thus, the electrochemical gradient ΔP consists of a membrane potential $(\Delta \Psi_{\rm m})$, also called voltage, and a pH gradient $(\Delta \mu^{\rm H+})$ with the pH gradient typically less significant: $\Delta P = \Delta \Psi_m + \Delta \mu^{H+}$. The mitochondria maintain a membrane electrochemical potential

function is of about 150 mV.⁷ This electrochemical gradient (ΔP) is a source of potential energy for multiple mitochondrial functions, the most important being the driving of the ATP synthase (complex V) to condense ADP + P_i to generate ATP. Respiration of isolated mitochondria is commonly studied

Respiration of isolated mitochondria is commonly studied by the sequential addition of substrates and specific respiratory complex inhibitors. NADH-linked substrates such as pyruvate and glutamate feed electrons through complex I while succinate feeds electrons into complex II. The addition of these substrates results in electron transport, increased ΔP , and oxygen consumption known as state II respiration. The addition of ADP activates complex V to deplete ΔP and increase the rate of oxygen consumption known as state III respiration. Depletion of the ADP returns the respiration to the pre-ADP state known as state IV respiration. The addition of a compound such as carbonyl cyanide *m*-chlorophenylhydrazon (CCCP) depletes the electrochemical gradient resulting in maximal "uncoupled" respiration. The different steps of

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The mitochondrial inner membrane is highly in-folded into double membrane structures known as cristae. These cristae are closed at the intersection with the intermembrane space between the inner and outer mitochondrial membrane to create closed cristae lumens.⁸ The ETC pumps the protons into the cristae lumens on which the ATP synthases are bound.^{9,10} Cleavage of Optic atrophy-1 (OPA1), which is located at the site where the cristae lumen is closed, releases the protons and disrupts the coupling between the ETC and ATP synthase.⁸ The mitochondrial system is important for multiple other mitochondrial functions including mitochondrial membrane dynamics, thermogenesis, Ca²⁺ homeostasis, redox signaling, and apoptosis.^{11,12}

Mitochondria ultrastructure has been extensively characterized with transmission electron microscopy (TEM) and CryoTEM in fixed cells.^{13–18} However, only by imaging functional, intact mitochondria can one ascertain information about the electrophysiology of the organelle. Because the cristae are about 100 nm wide, they cannot be studied with diffraction-limited microscopy. Recently, this limitation is being addressed using super-resolution microscopy.

Super-resolution optical microscopy of fixed cells has been deployed extensively to study cristae structure and membrane protein distributions along the membrane.¹⁹ But to understand the physiology of individual mitochondria, super-resolution of functional, intact mitochondria is required. Recent studies have employed super-resolution microscopy on mitochondria in live cells.²⁰⁻²³ To put this work into proper context, all but one of the previous works has been on structure, not function (i.e., voltage). Although they are intimately linked, function is much more important (and difficult to measure) because, after all, life is function, not structure. Only one of these papers studied mitochondrial electrophysiology (function) using a membrane sensitive lipophilic cationic dye, and they completely misinterpreted the relationship between the dye fluorescence and membrane voltage, and did not perform the battery of metabolic manipulations possible with isolated mitochondria, as they used whole cells. A lipophilic cationic dye diffuses freely from one side of a membrane to the other, since the hydrophobic side groups give it good solubility in the interior of the lipid bilayer. No channel or energy consumption or redemption is required to allow passage of the dye. At low concentrations, the charge does not affect the membrane voltage, and the dye accumulates on one side or the other because thermodynamics says the probability of a particle being in a given state is proportional to $e^{-}(energy/kT)$ of that state. Therefore, the ratio of dye concentrations is given by the Nernst equation, discussed in more detail below. However, many previous studies incorrectly assumed all the dye was free, neglecting the membrane binding of the dye, which has long been known to be the most significant component of the total dye fluorescence.²⁴ For example, our studies in 2010^{25,26} on isolated mitochondria using tetraphenyl phosphonium lipophilic cation (TPP⁺), detected electronically (rather than optically as in this study), used a calibration routine to convert to membrane potential that assumed (based on work by Kamo²⁷ others) that the total amount of TPP⁺ on the matrix side was approximately 90% bound to the inner membrane, and 10% free. Other groups later²⁸ used the same procedure, which lumped the membrane binding into an "activity

coefficient" that combined free and membrane bound dye since they could not (until now) be resolved at that time. We²⁹ and others (e.g.,³⁰) that previously used diffraction-limited microscopy to image voltage dye concentration (Tetrame-thylrhodamine, Ethyl Ester, TMRE) were not able to resolve the cristae and therefore did not have any images showing membrane localization.

To characterize differences in the physiology of individual mitochondria from cells, we report here procedures for characterizing the mitochondrial structure and function of isolated, functional mitochondria using super-resolution microscopy. This revealed that we can use super-resolution quantification of mitochondrial membrane potential using lipophilic cationic dye fluorescence to characterize the respiratory function of individual isolated, functional mitochondria in a way not possible in whole cells, potentially permitting elucidation of differences between individual mitochondria. Finally, by careful analysis of structure dyes and voltage dyes (lipophilic cations), we demonstrate that most of the fluorescent signal seen from voltage dyes is due to membrane bound dyes, and develop a model for the membrane potential dependence of the fluorescence contrast for the case of super-resolution imaging, and how it relates to membrane potential. This quantitative voltage-dependent membrane binding model explains why super-resolution images of lipophilic cationic dyes show strong intensity near the cristae and not in the matrix. This model enables quantitative imaging of super-resolution voltages inside functional, intact mitochondria with super-resolution.

LOGICAL STRUCTURE OF THE PAPER

This paper is organized into three major sections. In the first section, we develop and validate a quantitative model to demonstrate voltage imaging with super-resolution microscopy. In the second major section, we apply this to mitochondria in different metabolic states. In the third section, we discuss the need for biophysical models of mitochondrial function based on the Poisson statistics that results from the # of hydrogen ions in the cristae.

In the first section, we demonstrate that vital, isolated mitochondria voltages and ultrastructure can be imaged with super-resolution microscopy. These are the super-resolution images of vital isolated mitochondria. Next, we demonstrate that the voltage dye is not free in the mitochondrial matrix but rather bound to the membranes, albeit in a voltage dependent manner. This finding contradicts prior, incorrect interpretations in some of the literature assuming that the dye is free and unbound, and requires a model to interpret the voltage imaging since the old model is wrong. Next, we develop and apply a model originally developed for diffraction limited micrsocopy (where the entire organelle appeared as one voxel, and the imaging technology could not localize the voltage dye within the organelle), and use this to quantitatively interpret and explain the voltage images we obtained. This model completely and consistently takes into account membrane binding. Next, in order to test our proposed model to more conditions, we use the model to make predictions about what would be observed in the absence of a membrane potential (e.g., created by CCCP) and to predict the fluorescence intensity inside the matrix of the small amount of free (unbound) voltage dye. These are unusual conditions which researchers usually do not investigate in detail. Sure enough, our measurements in these unusual conditions completely



Figure 1. Model and images of isolated mitochondria. (a) Model of mitochondrial membrane voltage.¹⁰ (b) Isolated mitochondria stained with membrane fluorescent dye, NAO (c) Isolated mitochondria stained with voltage-dependent dye, TMRE. A simple application of the Nernst equation. Scale bars show the resolution of various imaging technologies for the TMRE dye. Reprinted from Trends Cancer, 3 (12), Burke, P. J. Mitochondria, Bioenergetics and Apoptosis in Cancer, Pages 857–870. Copyright (2017). with permission from Elsevier.

confirm the predictions of our voltage dependent membrane binding model. With this comprehensive, quantitative, experimentally validated model, we have provided the foundation for all future studies on the voltage distribution in mitochondria measured with super-resolution microscopy.

In our studies, we used all 3 modern methods of superresolution microscopy: Airy, STED, and Lattice SIM (Structured Illumination Microscopy). While it is possible in some methods to observe clearly the outline of internal structure of mitochondria such as individual cristae, with voltage imaging, the resolution (of order 90 nm) is only able to observe cristae if they are separated, but cannot observe individual cristae in cristae dense mitochondria. We discuss this quantitatively in this section and demonstrate how the density of cristae, their voltage distribution, and the response to pharmacological manipulation of different metabolic states can be observed, even if individual cristae are not resolved.

The second major part of this paper aims to apply this model to mitochondria in different metabolic states, something not possible in whole cells. Therefore, this is the demonstration of super-resolution voltage imaging in mitochondria in different metabolic states. These findings both reproduce all of the classical biochemistry metabolic studies of mitochondria, as well as demonstrate changes in the spatial distribution of the voltages as a function of metabolic state.

In the third section, based on our observed experimental data in the first two sections, we model the proton distribution inside the cristae semiquantitatively based on the membrane potential, capacitance, and pH. We demonstrate that bulk models of pH need to be replaced by refined models of electrophysiology at the nanoscale in mitochondria.

RESULTS

Vital isolated mitochondria cristae structures and super-resolution electrical voltages can be resolved by super-resolution microscopy. The ultrastructure of the organelle can be imaged using membrane binding dyes such as Nonyl Acridine Orange (NAO), mitotracker green (MTG), mitotracker red (MTR), mitotracker deep red (MTDR), etc. In this work, we utilize these dyes to image the location of the membrane cristae within the limits of the resolution of the imaging system. (Although these dyes show some dependence on membrane potential,³¹ we only use Tetramethylrhodamine, Ethyl Ester (TMRE) for voltage imaging, as it is more studied, and better understood.) This is shown in Figure 1, where we have used super-resolution microscopy (Airyscan) with NAO to image the ultrastructure of a single mitochondrion isolated from a human cell line (Methods).

In order to quantitatively assay membrane potential, a lipophilic cationic dye is traditionally used. As the dye has lipophilic moieties, it is soluble in the hydrophobic interior of the lipid bilayer membrane, and can readily diffuse from one side to the other. Since it is charged, its location inside vs outside the mitochondria is dependent on the membrane potential $\Delta \Psi_m$. Motivated by the apparent success of this approach in previous literature,^{7,32,33} we seek to attain additional information about the spatial dependence of $\Delta \Psi_m$ within the organelle. In Figure 1C, we show the fluorescence intensity of the lipophilic cationic dye TMRE in an isolated mitochondrion. The cristae harboring the ETC transported protons are clearly giving rise to a nonuniform distribution of TMRE, and hence a very nonuniform voltage $\Delta \Psi_m$, along the organelle. Also shown in Figure 1C are scale bars indicating the spatial resolution of various imaging technologies. Thus, using the Airyscan microscope, we have succeeded in imaging the membrane potential of vital, isolated mitochondria.

How does one interpret these images in terms of the actual membrane potential/voltage and the TMRE dye? If one neglects binding to the membrane itself (discussed below), the difference in densities across the membrane would be governed by the Nernst equation:

$$n_i/n_o = e^{\wedge}(-q\Delta\Psi_m/k_BT)$$
(1)

where $\Delta \Psi_m$ is the membrane voltage, and n_i , n_o are the lipophilic cationic dye concentrations inside and outside the mitochondria (respectively), indirectly measured via the fluorescence intensity. A simplified application of the Nernst equation, using the background fluorescence (n_o) , indicates



Figure 2. Correlation of TMRE and NAO. (A) Naive model of TMRE uptake, neglecting membrane binding. If TMRE only exists as free molecules in the matrix, responding to the membrane potential $\Delta \Psi_m$ according to the Nernst equation (eq 1), then the TMRE intensity should be anticorrelated with the membrane dye NAO, in contradiction to what we observed. Line profile of (B) mitochondria in a HeLa cell and (C) isolated mitochondria, stained with TMRE and NAO. The voltage sensitive cationic dye TMRE is localized at the cristae membrane, as demonstrated by the correlation between the TMRE and NAO intensity peaks, in contradiction to the naïve model for free TMRE. (D, E) Summary of experimental observations of TMRE localization in mitochondria. mtDNA was shown to be in the dark regions through PicoGreen staining in a separate experiment. (F) Line profile of isolated mitochondria TMRE image before and after treating with 10 μ M CCCP.

varying voltages $(\Delta \Psi_m)$ along the mitochondria, near where the cristae are, indicating "high" voltages near the cristae. In addition, large dark regions seem to indicate low voltages in the mitochondrial matrix.

However, this interpretation (presented in, e.g., refs 20 and 34) is not correct, as it ignores membrane bound TMRE. For example in ref 20, it assumes free (unbound, diffusible) TMRE in "compartments" of mitochondria was being resolved, and neglected binding to the membrane, which has long been known to be a significant factor.²⁴ This is understandable because (1) many references (even recent ones^{20,34}) present the false picture that most of the TMRE are free on both sides

of the membrane and neglect membrane binding, and (2) to date (until the advent of super-resolution microscopy), imaging the membrane bound TMRE has not been possible.

Most of the voltage sensitive cationic lipophilic dye TMRE is membrane bound, not free. Our Airyscan images reveal that the TMRE fluorescence correlates with the distribution of the mitochondrial cristae, as detected by the cardiolipin binding dye NAO. This is confirmed by plotting a line scan of the intensity along the length of individual vital mitochondria showing the overlap between the TMRE and NAO fluorescence levels (Figure 2B and Figure 2C). We observe this in both whole cells (reproducing ref 20, which



Figure 3. Uptake model for TMRE staining of mitochondria for voltage imaging. (A) Four-compartment model, showing membrane binding on both sides as well as the inside and outside. (B) Potential profile. (C, D) Zero and finite voltage potential profile of the binding of TMRE. The green and blue circles show the free TMRE on the outside (buffer side) and inside (matrix side) of the mitochondria. The orange and red circles show the bound TMRE on the outside and inside of the mitochondria, respectively. (E, F) Zero and finite voltage localization of the TMRE, showing the difference in # of TMRE molecules in the different regions. At finite voltage, the most intense fluorescence would be expected from the TMRE molecules indicated by the pink dots, localized at the matrix side of the membrane. The other TMRE molecules (free in the matrix, free in the buffer, bound to the buffer side) would be much dimmer and possibly not even observed within the practical dynamic range limits of the fluorescence detection system used. At zero voltage, the overall intensity (averaged over the organelle) would be much lower, but the intensity distribution would still be expected to be highest near the membrane.

found the same without explanation), as well as isolated mitochondria. Given that the mitochondrial inner membrane thickness is 4 nm and in tightly coupled mitochondria the infolded membranes are tightly juxtaposed with a separation between 20 and 100 nm, we can estimate that a cristae finger would have a width of approximately 30 to 110 nm which is within the spatial resolution of the Airyscan microscope of 90–120 nm. Hence, this places the positively charged lipophilic dye in close proximity to the positive electromagnetic field of the cristae, an anomaly observed but not explained in a previous Airyscan study of mitochondria within the living cell.²⁰

To further confirm that the TMRE is not evenly distributed within the mitochondrial matrix, we stained the isolated mitochondria with PicoGreen which stains mitochondrial nucleoids green. Mitochondrial nucleoids are located in the mitochondrial matrix (Figure 2D), and the staining of isolated mitochondria with TMRE and PicoGreen confirmed that the TMRE fluorescence does not correlate with the position of the mtDNA nucleoids and thus does not occupy the mitochondrial matrix (Figure 2E).

The explanation for this observation is that the TMRE is bound to the membrane, something which has been known with indirect studies for a long time.²⁴ Here, voltage-dependent membrane bound lipophilic cationic dyes are being imaged in vital, isolated, intact, functional mitochondria, clearly and directly confirming via super-resolution microscopy that most of the TMRE are bound to the membrane, something that was only possible to determine via indirect methods previously.

Binding of the TMRE Dye to the Membrane Model. In order to properly interpret the images of the TMRE intensity related to the membrane potential, it is critical to include the bound TMRE in consideration. To do this, we use a model proposed by Rottenberg in 1984,³⁵ and shown in Figure 3A. Rottenberg³⁵ proposed this in the context of mitochondria, but this model has not been used to interpret super-resolution images until this work: "The accumulation of these cations by mitochondria is described by an uptake and binding to the matrix face of the inner membrane in addition to the binding to the



Figure 4. Isolated mitochondria TMRE signal in different respiratory states. (A) Mitochondrial structure in different respiratory states. The numbers on top of the figure represent the time in seconds. The pixel size of the image was 0.048 μ m, which is limited by the inherent limits of the microscope. (B) Averaged TMRE changes of single mitochondrion during respiratory state transitions. (C) Averaged TMRE changes of single mitochondrion during respiratory state transitions. (C) Averaged TMRE changes of single mitochondrion treated with Oligomycin and CCCP. Starting with 178 μ g/mL isolated mitochondria, quantified by the Bradford assay, we stained the mitochondria with 10 nM TMRE and collected images using time-steps of 5 s to avoid photobleaching. The succinate (2.5 mM) was added at the 10th second, and ADP was added at the 240th second and again at the 380th second, giving a final concentration of 250 μ M and 500 μ M, respectively.

cytosolic face of the inner membrane." Rottenberg used radiolabeled lipophilic cations (triphenylmethylphosphonium (TMTP⁺), tetraphenylarsonium (TPA⁺), and tetraphenylphosphonium (TPP⁺)) to determine the concentration in the buffer, and therefore no imaging was used. Kamo and Demura²⁷ used this model and detected TPP⁺ in the buffer with electrochemical sensors; again no imaging was used: "The membrane potential-dependent binding was analyzed with a

model: the membrane is split into two halves, outer and inner half, and the amounts of bound probes in each region are governed by the concentration in the contiguous solution." Follow on work by Scaduto²⁴ used TMRE and imaging, but not super-resolution imaging. We used diffraction-limited imaging also in mitochondria contained in nanofluidic chambers.²⁹ In this work, we extend the use of this model to interpret voltage

In this model, TMRE is bound on the matrix and buffer (cytosol) side of the inner membrane. The amount of bound TMRE on the matrix side is proportional to the free concentration on the matrix side. The amount of bound TMRE on the buffer (cytosol) side is proportional to the free TMRE concentration on the buffer (cytosol) side. At zero membrane potential, the inner and outer free concentrations are equal. At nonzero membrane potential, the inner to outer free concentration obeys the Nernst equation; i.e., there is a higher inner concentration. Therefore, there is also a higher amount of TMRE bound on the inner membrane. The amount of TMRE bound on the outer membrane stays the same. It has been known since 1999²⁴ that the amount of bound TMRE in the mitochondrial inner membrane is about 100× larger than the amount of free TMRE in the matrix (by mole #), regardless of the potential. Since super-resolution imaging can resolve the cristae, i.e. internal membrane structure, it is mostly the TMRE bound on the inner membrane that is imaged during fluorescence, as it is larger by mole # than the free TMRE in the matrix, and as it is more concentrated (on the surface vs diffuse) in space.

The biophysical basis of this model is shown in Figure 3. In this model, TMRE ions experience an effective potential energy profile (for zero voltage) shown in Figure 3B (from Rottenberg³⁵). The shape of this curve results from the competition between the lipophilic side groups encouraging insertion into the membrane, and the charge encouraging repulsion from the membrane.³⁵ Since both effects do not have the same spatial profile, this results in two minima in the potential, one at each side of the membrane, and thus two binding sites. The depth and width of the binding sites will determine the concentration of lipophilic cations in the membrane vs the free concentration: The concentration of free (unbound) ions in solution is proportional to the concentration of bound ions on the surface of the membrane. These constants of proportionality (defined as a₀ and a_i in Figure 3) must typically be measured empirically (see Supporting Information (SI) section 3).

In Figure 3C, this biophysical model is redrawn under zero and finite membrane potential, showing the TMRE densities bound to each side of the membrane, and free on each side of the membrane, and defining the binding coefficients (also referred to as activities in literature). We prefer the term binding coefficients instead of "activities" sometimes used in the literature, because it explicitly clearly states the physical meaning in this context. Until this work, it was not possible to visualize the location of the TMRE dye molecules in the membrane compartments in mitochondria. However, various indirect techniques have been demonstrated to quantify the membrane binding in this model (see SI section 3). Although Figure 3C is implicitly what has been used to interpret membrane potential assays on mitochondria in the literature,²⁵⁻²⁸ it has never been explicitly presented as we have done in Figure 3C. The reason is that, until the advent of super-resolution microscopy, it was not possible to image the bound and free TMRE components independently.

Using known rate constants/activity coefficients (see SI section 3), we show in Figure 3D schematically how the TMRE molecules would be distributed in space at zero and finite membrane potential in a hypothetical mitochondrial inner membrane. Under finite potential, the purple population (TMRE bound to the inner membrane) will create the most

fluorescence intensity. The free TMRE in the matrix (blue population) will be relatively dim. This is exactly what we observe experimentally (Figure 2). In sum because the # of TMRE molecules bound to the matrix side of the membrane is $\sim 100 \times$ larger than the number of free TMRE molecules inside the matrix, and because the membrane bound TMRE molecules are more concentrated on the surface of the membrane, it is the membrane bound TMRE on the inner membrane that "glows" in fluorescence images. This explains why, in our images, the cristae regions glow with TMRE but the matrix regions seem dark. A detailed accounting of the binding constants is presented in SI section 3.

Application of this model makes two additional predictions that we can test quantitatively: (1) The matrix region should not be completely dark, and (2) the membranes should still be labeled with TMRE even when the membrane potential is completely collapsed. We discuss these next.

TMRE stains the membrane even after the voltage is collapsed. When we collapsed the voltage using CCCP, the total intensity of TMRE averaged over the entire organelle seemingly dropped to zero (Figure 4C and Figure 2F). However, on closer investigation, we found that it did not completely drop (Figure 2G). In the arbitrary units used, quantitatively it dropped to 200 when it was 5000 under energized mitochondria. Using super-resolution microscopy, we could look closer at the distribution of the dye after the collapse of the membrane potential. This is shown in Figure 2F. Although the overall intensity is lower, the shape is still similar. The line profile confirms the cristae are still labeled with (bound) TMRE, albeit at a much lower intensity. Thus, prior studies which showed the TMRE collapse are consistent with this work. In addition, this confirms the application of the model we proposed above. These effects are reproducible in different cell lines (see SI section 11).

There is some TMRE fluorescence in the matrix. According to the model, the free concentration of TMRE (inside the matrix), though small, should be observed in both cases whether the membrane potential $\Delta \Psi_m = 0$ or not. This fits our observation in Figure 2F. The TMRE intensity in the matrix, in arbitrary units used, was nonzero even after CCCP collapsed the voltage.

Postfacto Justification To Use Nernst Equation in **TMRE Imaging Studies.** At zero voltage, the bound TMRE is split roughly 50/50 on the inside/outside binding site. At finite voltage, the TMRE bound to the outside stays the same, but the TMRE bound to the inside is larger by a factor of $e^{(-q\Delta\Psi_m/k_BT)}$. For a typical membrane voltage of 150 mV, this is a factor of 400. Therefore, at finite voltage, the intensity of fluorescence is dominated by the TMRE bound to the matrix side of the membrane. In this way, the Nernst equation can be used as a semiquantitative measure of the local voltage of the membrane. Furthermore, it can even be used to determine the local voltage. Only when the voltage gets low compared to kT does this approximation break down. This postfacto justifies the use of the Nernst equation to image the membrane voltage in super-resolution microscopy studies of live cells and mitochondria, and studies where only the total uptake of TMRE is measured, which was the case for all studies until our super-resolution study. This means future researchers can use the Nernst equation in super-resolution studies of mitochondrial membrane potential with this justification, but the interpretation should include rather than ignore the



Figure 5. Schematic diagram of several different species and their distribution within a single cristae finger. Not shown are the OH- species on the membrane needed to maintain charge neutrality.

membrane binding, quantitatively modeled in this paper in the context of super-resolution microscopy.

CONCLUSION

High spatial resolution cristae electrophysiology during different metabolic states can be studied with isolated mitochondria using super-resolution microscopy. Based on the correct interpretation of Rottenberg's 1984 membrane binding model,³⁵ we can now quantitatively study mitochondria super-resolution electrophysiology and ultrastructure in different metabolic states. Motivated by the original observation by Hackenbrock^{16,17} that mitochondrial morphology changes in response to metabolic status (measured via TEM), we aimed to determine if the electrical voltage distribution also changed. We imaged the membrane potential (via super-resolution imaging of the TMRE fluorescence intensity) of intact, functional isolated mitochondria under different respiratory states, using pharmacological manipulation of the electron transport chain. Figure 4A shows the time-lapse super-resolution images of mitochondria in different respiratory states. In this study, we fed electrons into the ETC through complex II using succinate as the substrate to initiate state II respiration. We then added ADP to initiate state III respiration which on completion of ADP phosphorylation resulted in state IV respiration.7 This is the real-time, live image of the voltage changes in mitochondria with the

ultrastructure clearly resolved, as the mitochondria are put into different metabolic states.

Using this method, we demonstrate that the TMRE fluorescence intensity (indicative of local membrane potential $\Delta \Psi_m$) is bright in both metabolic states, getting brighter in state IV (defined as the presence of substrates but without ADP hence without ATP synthesis), and getting dimmer when ADP is present (due to the synthesis of ATP consuming some of the energy stored in the membrane potential). Furthermore, we show clearly that the dark regions remain dark in both metabolic states. This clearly indicates that the primary binding site of the fluorophore is at the cristae, when it comes to electrical voltages, regardless of the metabolic state.

Figure 4B shows the average TMRE fluorescence intensity over the entire organelle (defined as a region-of-interest (ROI) as discussed in the Methods section and SI section 7) as a function of time, under different buffer chemistries designed to manipulate the ETC and, thus, the mitochondria membrane potential. The implicit assumption is that the TMRE average so determined can be used as n_i in the Nernst eq 1 to determine the $\Delta \Psi_m$ average.

Consistent with the expectations from standard respiration studies,⁷ including our studies with external TPP⁺ electrodes which corroborated the findings,^{25,26} succinate addition increased TMRE fluorescence indicating the rise in mitochondrial membrane potential (Figure 4C). Addition of ADP caused a decline in TMRE fluorescence indicative of the utilization of the membrane potential by the ATP synthase to

convert ADP to ATP, and when the phosphorylation of ADP was complete and the ATP synthesis stopped, the TMRE fluorescence increased due to the recovery of the membrane potential via state IV respiration. A second addition of ADP repeated the state III to state IV progression.

Additionally, to confirm prior results still apply in our measurements, we showed that oligomycin causes the TMRE fluorescence to increase (indicating that the average membrane potential increased): Inhibition of the ATP synthase with oligomycin drives the mitochondrial electrochemical gradient to its maximum resulting in maximum TMRE uptake and fluorescence. Prolonged oligomycin exposure caused the membrane potential to decline, a phenomenon commonly observed, perhaps due to the activation of the mitochondrial permeability transition pore (mtPTP). Furthermore, we showed that, with the addition of CCCP, the average TMRE fluorescence drops close to zero: Treatment with the mitochondrial uncoupling agent CCCP collapses the inner membrane electrochemical gradient resulting in the release of the mitochondrial TMRE and minimal mitochondrial fluorescence. Hence, with intact, functional mitochondria, the uptake and release of TMRE follow the expectations of changes in the mitochondrial membrane potential during OXPHOS function. This is reproducible over all 4 cell lines studied (see SI section 12). Additionally, mitochondrial heterogeneity as well as spatial and temporal fluctuations can be further analyzed (see SI section 16).

DISCUSSION

Bulk models may break down in the cristae: There is only one (calculated) H⁺ ion in the cristae solution at known pH values, but electric fields are extremely intense. We now discuss the distribution of various charged species near a single cristae finger (Figure 5). Note that this is for discussion purposes only and does not detract from the main result of the paper that TMRE is localized on the matrix side of the mitochondrial inner membrane when there is a sustained membrane potential. In this discussion, we seek to put into perspective the electric fields, pH, and ionic species of the mitochondria as a whole organelle, from a systems perspective, and to indicate schematically what the TMRE fluorescence images represent physically.

We first discuss TMRE distribution. As discussed above, at the TMRE concentration used, the TMRE charge density is small compared to the other ionic species. Therefore, the TMRE does not significantly change any electric fields; rather it only acts as a probe of those fields and responds to them. Approximating a single cristae finger as a cylinder of radius 100 nm and length 500 nm for volume and surface area estimates, and using known binding constants discussed in detail above and in the Supporting Information, based on a membrane potential of 150 mV, we find there will be ~1,000 bound TMRE molecules at the surface on the matrix side of a single cristae finger (red dots). These give the dominant observed fluorescent signal in super-resolution images. The TMRE is positively charged, so there will be ~ 1000 negative charges on the other side of the membrane (cytosol/buffer side), presumably OH⁻ species (not shown). The remaining TMRE is small in number and difficult to observe in superresolution images: In the matrix, there will be ~ 10 free TMRE molecules in the field of view (blue dots). Inside the finger, there will be less than one free TMRE molecule (green dot)

and less than ~ 10 bound TMRE molecules (orange dots) on the cytosol/buffer side of the membrane.

We turn next to the unbound hydrogen H⁺ and OH⁻ species. We assume the pH = 7.2 in the cytosol/buffer. Because protons are pumped out of the matrix, the matrix must be at a higher pH than the cytosol/buffer. While the exact matrix pH is difficult to measure, it is generally accepted to be between 7.4 and 8 (corresponding to a delta pH across the mitochondrial membrane of somewhere between 0.2 and 0.8 pH³⁶⁻⁴¹). The intermembrane space (IMS) has a lower pH than the cytosol. Although not exactly known, these are indicated as 7.2, 6.8, and 8.0 in the cytosol (buffer), intermembrane space (IMS), and matrix, respectively, in the figure. We and others³⁹ have shown that protons are concentrated in the cristae fingers since the OPA1 and MICOS complexes block proton transport through the tight cristae junctions. Since the source of the protons is dominantly inside the cristae fingers where the components of the ETC are localized,¹⁰ the effective pH inside the finger would be lower than the IMS, i.e. lower than 6.8. In order to estimate the # of protons inside a single finger, we estimate the volume as a cylinder of diameter 100 nm and length 500 nm. Based on this, if the pH inside the finger is 6.5, there will be statistically about one H⁺ ion in one cristae. Since the application of the concept of pH assumes a statistical distribution of a large number of OH⁻ and H⁺ ions, its application to a volume with less than one H⁺ ion indicates that a model is needed.

We now turn to bound hydrogen H⁺ and OH⁻ species. Since there is a membrane potential of around 150 mV across the membrane, by Gauss's law of electrostatics, there must be a sheet of positive charge on the inside of the cytosol/buffer side of the membrane (pink area), and a corresponding sheet of negative charge on the matrix side of the membrane (blue area). Based on an estimated bilayer capacitance per unit area of 1 μ F/cm², the amount of charge can be estimated as one electron equivalent of charge per nm^2 , positive on the cytosol/ buffer side of the membrane, negative on the matrix side of the membrane. We postulate that the molecular identity of positive charges on the cytosol/buffer side are H⁺ ions, since these are the ions that are actively and continuously being pumped by the ETC to maintain the membrane potential. Approximating the total surface area of a single cristae finger's membrane as a cylinder of radius 100 nm and length 500 nm, the number of estimated charges per cristae finder is 10,000 (shown as yellow circles with a plus sign). Similarly, there would be 10,000 OH⁻ charges on the matrix side of the membrane (not shown).

The electric fields inside the cristae are intense. This huge imbalance between one free H⁺ ion and 10⁵ on the surface must affect the electrostatics inside the cristae to create immense electric fields. This would also have a huge potential to impact the protein complexes in the ETC. Clearly, a model, not based on bulk, continuum distributions of charge and pH, which takes into account the immense electric fields and their impact on the ETC performance under different metabolic conditions is needed. The recognition of the few # of protons in a mitochondrion was also recently pointed out by Silverstein.⁴² Development of theories and experiments in this "stochastic" limit has begun in test systems.^{43,44} It has been shown that the classical definition of pH in very small volumes needs to be revised when applied to fluorescent probes of pH in mitochondria.⁴⁵ Our super-resolution studies represent a significant step in experimentally dissecting the superresolution electrophysiology of this organelle.

It is not unreasonable to speculate that, even given the Debye screening length of a few nanometers, at least in some regions of the cristae, the effective pH is not 6 or 7 but much more acidic, even approaching pH 1.^{46,47} One might even speculate even further that these strong fields affect the spin polarization and may even give rise to quantum effects in the microscopic environmental chemistry or even the macroscopic phenotype. Hints of this have already been reported in the literature.⁴⁸ While in their infancy, super-resolution studies such as these, combined with quantum probes of mitochondrial function,⁴⁹ may enable powerful methods of probing the connection between energy and life.

MATERIALS AND METHODS

Cell Culture and Fluorescent Dye Staining. The MB231 cells and HeLa cells used in this research were purchased from ATCC. The HEK293 cells and HK2 cells were gifts from a collaborator. All the cells were cultured for 2–3 days in 75 cm² tissue flasks at 37 °C and 5% CO₂ before being ready for experimentation. Dyes (10 nM TMRE or 100 nM MitoTracker DeepRed (MTDR) and 100 nM MitoTracker Green (MTG) or 100 nM 10-N-nonyl acridine orange (NAO) or 3 μ L/ml PicoGreen; Santa Cruz Biotechnology) were added to the cell culture media and incubated 1 h prior the cell retrieval.

Mitochondrial Isolation. After retrieval, the cells were transferred into a falcon tube with 1 mL of ice-cold RBS buffer (5 mM KCl, 1 mM MgCl₂, 20 mM HEPES (pH 7.0)) added, and the tube was then incubated on ice for 10 min. After incubation, the solution was transferred into a glass homogenizer, and we performed 20 strong strokes separately using a loose and tight stroker. After the douncing procedure, 1 mL of homogenization buffer (450 mM Mannitol, 150 mM Sucrose, 1 mM EGTA, 40 mM HEPES, 1% (w/v) fatty-acid free BSA, 2% protease inhibitor) was added to the solution. Next, we centrifuged the homogenate at 1000g for 5 min at 4 °C to remove large-scale debris. The supernatant was recentrifuged at 12000g for 20 min at 4 °C to get purified isolated mitochondria. The pellet was collected and resuspended in 37 °C KCl buffer (140 mM KCl, 2 mM MgCl₂, 10 mM NaCl, 0.5 mM EGTA, 0.5 mM KH₂PO₄, 2 mM HEPES) (pH 7.2).

Live Isolated Mitochondria Imaging. The collected isolated mitochondria were resuspended in 37 $^{\circ}$ C KCl buffer and plated in CELLview 4-compartment glass-bottom tissue culture dishes (Greiner Bio-One, 627870), PS, 35/10 mm. A 1500g, 8 min centrifugation step was applied prior to isolated mitochondria imaging to spin down the isolated mitochondria to the bottom of the dish. To improve the attachment of isolated mitochondria, the dishes were coated with Poly-L-lysine (0.1 mg/mL) for 10 min. Later, we removed the solvent and put the cartridge in a fume hood for 20 min to dry up before use. Prior to image analysis, raw .czi files were automatically processed into deconvoluted Airyscan images using the Zen software.

Protocols for Visualization of Mitochondria Structure Using Airyscan and STED Microscopy. For Airyscan: We used a Zeiss LSM900 (w/incubation chamber, set to 37 °C) with Airyscan with an alpha Plan-Apochromat 63×/1.4 Oil DIC M27 objective. We adjusted the laser power between approximately 0.3% to 2%, and the master gain between 750 and 900. We started continuous scanning at maximum speed at a zoom factor of 1, in order to obtain a relatively strong signal-to-noise ratio for imaging. Later, we brought the field of mitochondria of interest into view and stopped scanning. We selected a mitochondrion of interest and used the crop function to zoom in approximately 6.0× to 10.0× until getting clear images of cristae structures. The pixel dwell time was set between 0.85 and 1.04 μs , respectively to avoid overtime exposure of mitochondria to the laser. Note that to get clear enough isolated mitochondria images, we set the frame time to no longer than 400 ms to avoid blurring due to the movement of mitochondria. NAO and MTG were used for structural imaging (labeling the lipid bilayer), and TMRE was used for voltage imaging, as explained in the main text.

For STED: We used an Abberior Stedycon (w/incubation chamber, set to 37 °C), gracefully on loan for a demonstration from Abberior. After obtaining a relatively strong signal-to-noise ratio at a zoom factor of 1, we brought a single mitochondrion into view and stopped scanning. We used the crop function to zoom in on the image to the desired size. We used the autoadjust function to find the best pixel size and pixel dwell time for the observation. The best pixel size and pixel dwell time in our experiment were 25 nm and 10 μ s, respectively. MTDR was used for structural imaging (labeling the lipid bilayer), and TMRE was used for voltage imaging, as explained in the main text.

Respiration State Experiment. Isolated mitochondria from HeLa cells were incubated in warm KCL buffer (140 mM KCl, 2 mM MgCl₂, 10 mM NaCl, 0.5 mM EGTA, 0.5 mM KH₂PO₄, 2 mM HEPES) with a temperature control setting to 37 °C once isolated from HeLa cells (State 1). The concentration of isolated mitochondria was measured by using the Bradford assay. The timestep for each image was 5 s to avoid photobleaching. The 2.5 mM Succinate was used as the substrate to trigger electron transfer (State 2) and 250 μ M ADP was added later to initiate the ADP-stimulated respiration (State 3).

Image Analysis. Processed Airyscan images were analyzed using ImageJ (Fiji) software. For all images performed in this draft, we only adjust the brightness and contrast to demonstrate relevant changes in structure. Images acquired with STED microscopy were deconvoluted using Huygens deconvolution software. Additional image analysis is described in detail in SI section 7.

ASSOCIATED CONTENT

Supporting Information

The Supporting Information is available free of charge at https://pubs.acs.org/doi/10.1021/acsnano.3c02768.

Respiration run images (ZIP)

Respiration run videos (ZIP)

Section 1: Phototoxicity/photobleaching. Section 2: Tubular vs Circular mitochondria. Section 3: How the binding constants were measured in the literature. Section 4: Airyscan and STED give comparable resolution for TMRE voltage stains. Section 5: Isolated mitochondria from different cell lines. Section 6: Confirmation that the mitochondria isolated are of optimal function and well coupled. Section 7: Image analysis and conversion to the average fluorescence intensity of TMRE over mitochondria. Section 8: State 3/State 4 average intensity plots. Section 9: The standard deviation of the TMRE fluorescence intensity. Section 10: 3D projection. Section 11: Distribution of the dye after the collapse of the membrane potential (other cell lines). Section 12: Response to oligomycin and CCCP is reproducible among cell lines. Section 13: Experimental conditions: Yield and statistics. Section 14: Relationship to Murphy et al. Section 15: Biological Implications: Disease and health in mitochondria. Section 16: Spatial and temporal statistical properties and mitochondrial heterogeneity. Section 17: Resolution discussion. Section 18: Comparison between Airyscan, STED, and Lattice SIM microscopy. Section 19: Wide view of isolated mitochondria: "Zoom out" vs "Zoom in". Section 20: Literature review for super-resolution live-cell imaging of mitochondria. Section 21: Chemical structure of fluorescent dyes used in this manuscript. Section 22: Confusion on the binding abounds in the literature. Section 23: Alternative methods to determine concentrations of dye inside and outside the mitochondria. Section 24: Relationship to Miller et al. (PDF)

AUTHOR INFORMATION

Corresponding Author

Peter J. Burke – Department of Electrical Engineering and Computer Science, University of California, Irvine, California 92697, United States; o orcid.org/0000-0002-8883-1014; Email: pburke@uci.edu

Authors

ChiaHung Lee – Department of Biomedical Engineering, University of California, Irvine, California 92697, United States

Douglas C. Wallace – Center for Mitochondrial and Epigenomic Medicine, Children's Hospital of Philadelphia and Department of Pediatrics, Division of Human Genetics, University of Pennsylvania, Philadelphia, Pennsylvania 19104, United States

Complete contact information is available at: https://pubs.acs.org/10.1021/acsnano.3c02768

Notes

The authors declare the following competing financial interest(s): Two authors are founding a company related to microfluidic mitochondrial assays.

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Supporting Information

Super-resolution imaging of voltages in the interior of individual, vital mitochondria

ChiaHung Lee‡, Douglas C. Wallace⁴, Peter J. Burke^{†*}

[†]Department of Electrical Engineering and Computer Science, ‡Department of Biomedical Engineering, University of California, Irvine, California 92697, United States

^ACenter for Mitochondrial and Epigenomic Medicine, Children's Hospital of Philadelphia and Department of Pediatrics, Division of Human Genetics, University of Pennsylvania, Philadelphia, PA 19104, United States

*Corresponding Author: pburke@uci.edu

Section 1: Phototoxicity/photobleaching

Both phototoxicity and photobleaching were observed in experiments for this work. A detailed and comprehensive study of these effects is beyond the scope of this paper and will be presented in a separate manuscript (Lee, et al, manuscript in preparation). For this work, only data where phototoxicity and photobleaching were not observed are presented.

Section 2: Tubular vs. Circular mitochondria

In cells mitochondria are generally tubular, they typically end up round when purified. The reasons for this are discussed in another manuscript (Lee, et al, manuscript in preparation), which is beyond the scope of this paper. Briefly, the mechanical lysis causes damage resulting in spherical mitochondria, but we have developed a gentler technique in which a fraction of the isolated mitochondria are tubular. For a statistical analysis of the fraction of tubular vs. spherical mitochondria, the reader is referred to Tables 1,2 and Section 13 in supporting information.

The tubular mitochondria are believed to be most representative of the mitochondria in cells, and so are the ones studied in this paper. The data on the circular mitochondria is beyond the scope of this paper, and will be presented in another manuscript (Lee, et al, manuscript in preparation).

Section 3: How the binding constants were measured in the literature

The electron spin resonance spectra of certain spin labeled lipophilic cations depend on whether the cation was bound or free. This was used to measure the amount of bound vs. free cation in liposome suspensions in 1978¹, for zero voltage and the controlled voltage across the liposome. This proved that the amount of bound cation was voltage-dependent. Furthermore, measurements showed that the rate/binding constants were such that the amount of bound cation (by mole #) was much larger than that free and inside the liposome, by at least an order of magnitude.

The rate constants and binding were quantitatively measured in mitochondrial suspensions in 1987 by Kamo² for tetraphenylphosphonium (TPP⁺) lipophilic cations: By using electrochemical detection of the TPP⁺ concentration in the buffer under various conditions, the authors were able to show that, similar to the liposomes, 1) the amount of TPP⁺ cation bound to the mitochondrial membrane was voltage-dependent, and 2) the number of TPP⁺ molecules bound to the mitochondria (matrix). A similar series of experiments used TMRE (as we do) and optical detection of the amount in the buffer to find the quantitative rate constants for mitochondria³. They found that, at 28 °C, the ratio of # TMRE molecules bound to the inner membrane to the # of TMRE molecules free in the inner matrix was 60, and 129 for the similar ratio for the outer membrane binding (buffer side). (See units discussion in supporting information.)

A detailed description of the binding model

The TMRE is assumed to be low enough density (at 10 nM) so that:

- The # of TMRE per surface area of the bilayer is not saturating all of the possible binding sites. (Large-density TMRE will saturate the binding, as shown in ^{2,4}.)
- The TMRE charge does not significantly perturb the electrostatics (electric fields), since other charged species such as H⁺, K⁺, Cl⁻, and OH⁻, are many orders of magnitude higher in concentration (μM to 0.1 M), and the fields generated by those charges is not changed much by the presence/absence of TMRE at 10 nM. That said, there will be some small OH⁻ or other negative charges to balance the TMRE positive charge.

The fundamental thermodynamic model regarding the binding of TMRE or any other lipophilic cation is based on the following assumption: The TMRE can move between different compartments, and the compartments are in equilibrium. The model used in this paper has four compartments, shown in Fig. 3.

Here, equilibrium means there is no net change in the average TMRE concentration with time, although it may fluctuate about the mean. Thermodynamics considerations of the Gibbs Free energy ⁵ imply that the electrochemical potential is constant. (At zero membrane voltage, the electrochemical potential is the chemical potential). If the energy of each compartment was the same, this would mean that the density of TMRE is the same in each compartment. However, there is a potential well for bound TMRE (see Fig. 3 in the main text), indicating that the densities will not be the same, even though the chemical potentials are the same.

The "density" of TMRE in the bilayer membrane is defined as the # of TMRE molecules/volume of the membrane compartment. The volume of the membrane compartment is equal to the membrane surface area times the width of the compartment (indicated as δ in Fig. 3). This is a model, which will be compared to experiments presently (below).

We make the following definitions for the density of TMRE molecules: n_i is the free TMRE inside a liposome or in the case of mitochondria inside the mitochondria, i.e. in the region called the matrix. n_{bi} is the density of bound TMRE bound to the inside surface of the membrane (in the case of a liposome) or the inside i.e. matrix surface of the membrane (in the case of mitochondria). Similarly, n_o is the density of free TMRE on the outside of the liposome or (in the case of mitochondria) on the cytosol (in cells) or buffer (in isolated suspensions of mitochondria). n_{bo} is the density of TMRE bound to the outer membrane surface (in the case of liposomes) or the outer mitochondria membrane surface (cytosol or buffer side) in the case of mitochondria. The bilayer is not assumed to be symmetric.

We define a_0 as the constant of proportionality between n_0 and n_{bo} . Through the following equation:

 $n_{bo} = a_o n_o$ Similarly, for a_i : $n_{bi} = a_i n_i$ Our definition does not provide any sort of a microscopic model for the origins of a_o or a_i , other than the assumptions of thermodynamic equilibrium and the overall shape of the potential shown in Fig. 3. The bilayer is not assumed to be symmetric, so we do not assume a_o and a_i are equal. Our definition is for expositional clarity in this paper's context, and not a standard in the literature. We do assume a_o and a_i are constants regardless of the membrane potential. This assumption is implicit in all of the literature to date 1-3.

Various authors in the literature have provided microscopic models for the value of a_0 . Rottenberg⁴, instead of a_0 , used $K_{mo}\alpha_0$, where " K_{mo} is the ion partition coefficient for the external surface of the membrane and α_0 is a function of the external surface potential ψ_0 ". Note that the surface potential is NOT the membrane potential, and is assumed to be constant ⁶.

The units of a_o or a_i are dimensionless. However, in practice, one does not easily know, and cannot easily measure, the exact surface area of the lipid bilayer of a mitochondrion. Furthermore, one cannot easily know, and cannot easily measure, the width of the binding potential well (δ in Fig. 3). Therefore, one cannot easily know or measure the "density" n_{bi} or n_{bo} of TMRE in the membrane compartment.

Binding constant per mg of mitochondrial protein:

Case I: $\Delta \Psi_m = 0$:

The experimental quantity measured with regard to mitochondrial suspensions is the total amount of protein in mg. This is usually measured by the Bradford assay, which measures optical absorption at a specific wavelength and converts this to mg of mitochondrial protein using an agreed upon constant from the literature ⁷.

The inner volume of the mitochondria (matrix volume) is usually taken as 1-2 μ l/(mg of mitochondrial protein). From this, the total # of TMRE molecules can be estimated in the matrix, given the quantity of mitochondrial protein measured via the Bradford assay, and the density of TMRE (in moles/ μ l i.e. molarity). At $\Delta \Psi_m = 0$, the molarity of TMRE is the same on the inside (matrix) and outside (buffer), which is easily measured.

For a given amount of mitochondrial protein in mg, how many TMRE molecules are bound to the surface? This can be expressed as moles/(mg mitochondrial protein). For a given amount of mitochondrial protein in mg, how much "volume" of membrane binding compartment is there? (This would be in Fig. 3 the membrane surface area times δ .) This would be expressed as μ l/(mg mitochondrial protein).

Matrix side:

(Considering the matrix side first): Rottenberg⁴ defines "apparent internal partition coefficient" K_i as our a_i times the membrane volume V_{mi} per mg mitochondrial protein:

 $K_i \equiv a_i V_{mi} / (mg mitochondrial protein)$

With these units, for a concentration n_i of TMRE in the matrix, the # of bound TMRE molecules would be:

(eq. 1) # bound TMRE molecules (matrix side) = n_{bi} V_{mi} = $a_i n_i V_{mi}$ = K_i' (mg mitochondrial protein) n_i

From Rottenberg, 1984 ⁴:

The membrane volume occupied by the phospholipids on the matrix and cytosolic surface of the inner membrane is approximately half the volume of the total phospholipids of the inner membrane. Quite likely the lipophylic cations occupy only a fraction of this volume. While this volume fraction is unknown it is proportional to the total membrane volume and therefore to the membrane protein content which is routinely measured. In the applications that follow the apparent surface membrane concentration is expressed in units of nmol/mg protein. The units of the apparent partition coefficients K', $(nmol/mg \text{ protein})/(nmol/ \mu l)$, are therefore expressed in $\mu l/mg$ protein.

These units are confusing, but they are what Rottenberg⁴ chose to use, and also authors since then 1,2 have used this nomenclature. Similarly, the # of free TMRE molecules in the matrix can be expressed as:

free TMRE molecules (in matrix) = $n_i V_i$

Again, one does not know the internal volume V_i easily. However, since the inner volume of the mitochondria (matrix volume) is usually taken as 1-2 μ l/(mg of mitochondrial protein), one can calculate:

(eq. 2) # free TMRE molecules (in matrix) = $n_i V_i = (mg \text{ mitochondrial protein}) (2 \,\mu l/mg) n_i$

On comparison with the formula for the # of bound TMRE molecules, one can see the K_i ' has units of μ l/mg.

Rottenberg and other authors have expressed experimentally determined binding constants as K_i '.

In comparing eq. 1, 2, once can see that if $K_i' > 1-2 \mu l/mg$, more TMRE is bound to the membrane than is free in the matrix, i.e. the ratio is:

bound TMRE molecules (matrix side) / # free TMRE molecules (in matrix) = K_i' / (1-2 µl/mg).

Scaduto³ found, for TMRE at 28 C, $K_i' = 60$ (Table 1, Scaduto). This indicates 60x more TMRE molecules are bound to the inner membrane (matrix side) than free TMRE molecules in the matrix (at $\Delta \Psi_m = 0$).

Buffer side:

A similar line of definitions applies for binding to the outer side of the membrane (the buffer side):

 $n_{bo} = a_o n_o$

 $K_o' \equiv a_o V_{mo} / (mg mitochondrial protein)$

(eq. 3) # bound TMRE molecules (buffer side) = n_{bo} V_{mo} = $a_o n_o V_{m0} = K_o'$ (mg mitochondrial protein) n_o

In comparing eq. 1, 3, once can see that if $K_0' > 1-2 \mu l/mg$, more TMRE is bound to the membrane than is free in the matrix, i.e. the ratio is:

bound TMRE molecules (buffer side) / # free TMRE molecules (in matrix) = K_o' / (1-2 µl/mg).

Scaduto³ found, for TMRE at 28 C, K_i '= 129 (Table 1, Scaduto). This indicates 129x more TMRE molecules are bound to the outer membrane (buffer side) than free TMRE molecules in the matrix (at $\Delta \Psi_m = 0$).

Case II: $\Delta \Psi_m \neq 0$:

If $\Delta \Psi_m \neq 0$, the free concentration ratio is governed by the Nernst equation:

 $n_i/n_o = e^{(-q\Delta \Psi_m/k_BT)},$

From equation 3, the # bound TMRE molecules (buffer side) do not change from the $\Delta \Psi_m = 0$ value.

From equation 2, the # bound TMRE molecules (matrix side) do change from the $\Delta \Psi_m = 0$ value, and it becomes larger by the factor e^(-q\Delta \Psi_m / k_BT).

Both cases are shown for $n_0 = 10$ nM in Fig. 3.

Section 4: Airyscan and STED give comparable resolution for TMRE voltage stains

In order to better resolve the cristae voltages, we next turned to STED as a potential higher resolution solution. Airyscan functions by reducing the point spread function, while STED functions with a donut photobleaching. Depending on the conditions, Airyscan can have a resolution down to 90 nm ⁸ with Airyscan Joint Deconvolution. Our implementation had a theoretical resolution of 120 nm because we had not yet upgraded to the 90 nm option.

In principle, STED can have a much better resolution, down to 20 nm ^{9,10}. Note that STED is very dependent on the bleach pump intensity and dye characteristics, while Airyscan is not. For this reason, it has been believed that Airscan is gentler on mitochondria, which are particularly sensitive to phototoxicity. However, it is possible to perform STED on live cells and mitochondria, at least for short periods of time. We decided to investigate the resolution of these two approaches on our isolated mitochondria.

We have performed STED and Airyscan imaging on mitochondria isolated using the same protocol (other than the imaging technology), in order to compare the two approaches. For structural studies, the resolution of STED was significantly better than Airyscan (Fig. S 1). The Full-width-half-maximum (FWHM) analysis gave us a 140 nm resolution of Airyscan with NAO dye and an 80 nm resolution of STED with MitoTracker DeepRed (MTDR) dye. This is consistent with the two prior studies of mitochondria in cells which quoted the resolution $^{10-13}$, which found 50 nm and 80 nm, 35-71 nm, and 45 nm, respectively. Those studies did not approach the ultimate resolution of STED of 10 nm, presumably because the dyes were not optimized and the pump intensity needed to achieve those resolutions would have killed the cells instantly. Thus, for structural imaging STED is clearly outperforming Airyscan, in terms of resolution, for imaging of intact functional mitochondria.

In our work, we are more interested in functional assays. Since the mitochondria are intact and functional, they should sustain a membrane voltage, and we aimed to find the method with the best possible resolution. To our knowledge, at this time there is not a STED optimized lipophilic cationic dye that can image voltages with the full potential of STED. Therefore, we used TMRE for voltage imaging. Fig. S 1 shows a line profile of TMRE-labeled mitochondria imaged under nominally identical conditions, optimized for the specific method, for both Airyscan and STED. We find a FWHM of 140 nm and 145 nm for Airyscan and STED, respectively, indicating that both methods provide comparable spatial resolution for voltage imaging. Hopefully, future research on new voltage dyes that are more optimized for STED can improve the spatial resolution beyond this.



STRUCTURE (Membrane stain NAO/MTDR)

Fig. S 1. Line profile of mitochondria STRUCTURE image (A) NAO + Airyscan and (B) MTDR + STED. (C) Image resolution comparison on structure image (Normalized intensity, Full-width-half-maximum (FWHM)). Line profile of mitochondria VOLTAGE image with (D) TMRE + Airyscan and (E) TMRE + STED. (F) Image resolution comparison on voltage image (Normalized intensity, FWHM).

Section 5: Isolated mitochondria from different cell lines

We have also observed non-uniform TMRE distribution and cristae structure in 3 other cell lines (HEK293, MB231, and HK2). This indicates the phenomenon is reproducible across cell lines.



Fig. S 2. Mitochondria isolated from MB231, HEK293, and HK2 cell lines stained with Mitotracker green and TMRE.

Section 6: Confirmation that the mitochondria isolated are of optimal function and well coupled

Mitochondria are notoriously tricky to harvest from cultured cells (especially those with a low mitochondrial complement such as HeLa). Additional proof is required that what resulted was actually mitochondria and not another cell fraction. The standard method to confirm organelles are functional and well coupled is to perform respiration measurements. Therefore, to confirm that the mitochondria are of optimal function and well coupled, we performed respiration measurements matching the conditions used for microscopy (37 °C, ambient, see Method).

To quantify organelle integrity, the respiratory control ratio (RCR) is usually used ^{6,14}. This empirical parameter is based on the observation that mitochondria damaged during isolation show an increased proton leak of the inner membrane as compared to undamaged mitochondria, hence an increased state 4 respiration rate. The RCR is typically defined as the ratio of the state 3 to state 4 respiration rate (achieved using different substrates for the electron transport chain). The RCR assay thus measures the "leakage" of membrane potential quantitatively: Higher RCR means less damage to the mitochondria during the isolation process.

There is no 'correct' value for the RCR; depending on the tissue and the substrate, values can vary from 3 to 15 or more for well-prepared mitochondria ⁶. We used an Agilent Seahorse XFe24 analyzer to measure the oxygen consumption rate (OCR) of mitochondria isolated using the protocol ¹⁵. Our RCR value of isolated mitochondria from mice heart tissue is 3.9 ± 0.7 and the RCR value of isolated mitochondria from HeLa cells is 2.37, the error bars are according to the measurements of multiple wells. These data matched with historical literature consensus values to demonstrate that mitochondria are functional and are derived from proper isolation.



Fig. S 3. The oxygen consumption rate of isolated mitochondria from mouse heart tissue. The calculated RCR =3.9.



Fig. S 4. The oxygen consumption rate of isolated mitochondria from the HeLa cell line. The calculated RCR = 2.37.

Section 7: Image analysis and conversion to the average fluorescence intensity of TMRE over mitochondria

The Zeiss microscope created a time-lapse series of images (snapshots in time), typically one image per second. The exposure conditions and time-lapse rates for each experiment are listed in detail in the tables below.

These images were processed by the Zeiss software using the Airyscan algorithm on the signal from each photodetector. The resultant file was an image file (CZI format, which is a Zeiss format) which contained the processed time-lapse images, one image per frame.

Since typically more than one mitochondrion was available within the field of view, we used ImageJ to manually select a rough (rectangular) region of interest around the mitochondria and save this as a TIF file with several hundred frames. These TIF files are provided as supporting information files (*Run_respiration_exp#_mito#*, where *#* indicates the number of the experiment and mitochondrion) and can be viewed as movies by appropriate viewers. To be clear, these TIF files have no image processing or adjustment, they are just the original image series in Zeiss CZI cropped and converted to TIF. No information was lost or gained in this process. Thus, the TIF files are indeed the "raw data".

We wrote a script in Igor (an analysis program available for Mac or PC) to process the images. The script calculated the average intensity above a certain threshold for each frame, and then plotted that vs. time. It also calculated the std. deviation of the intensity for each frame and plotted that vs time. Pixels below the threshold were assumed to be outside of the physical region of the mitochondria. This was confirmed manually. Finally, every 6 points were averaged to give the average intensity over that period (30 seconds) and plotted. Fig. S 5 below shows the raw calculated FI and the data averaged every six points. Any reader with Igor can run this script ("macro") to reproduce the figures in this paper ("processed data") from the provided TIF movies ("raw data").



Fig. S 5. Grey points are the average fluorescence intensity of the mitochondria for each frame. Black points combine 6 frames per point to show long-term trends.

Image processing script

```
Macro loadZeissTif(imagewavename, filename, pathname, Thre)
       // This macro loads Tifs timelapse from the Zeiss
       // PJB 12/20/2022
       // Add Threshold
       // CHL 12/28/2022
       String imagewavename // Wavename of image loaded
        String fileName // name of file to load or "" to get dialog
        String Pathname // name of path or "" get dialog
       Variable Thre // Threshold, give Thre=0 not to set threshold
        Silent 1; PauseUpdate
        Preferences 1
        variable m rows, m columns, m layers, m chunks // size of each
dimension of loaded waves
        // load the image
        ImageLoad/o/T=tiff/S=0/C=-1/Q/N=$imagewavename/p=$pathname filename
        // get size of image
       m rows=dimsize($imagewavename,0)
        m_columns=dimsize($imagewavename,1)
        m layers=dimsize($imagewavename,2)
        m chunks=dimsize($imagewavename,3)
        print "rows, columns, layers, chunks"
       print m rows, m columns, m layers, m chunks
        // make image waves
        imagetransform /p=3 getplane
                                       $imagewavename
        Display; DelayUpdate
        AppendImage M ImagePlane
        imagetransform /p=7 getplane
                                       $imagewavename
        //without threshold
        String m newwavename // name of 2d image wave for a particular frame
        String m avg wavename // name of wave with averages FI of images
        String m stdDev wavename // name of wave with std dev FI of images
        String m avg wavename dec // name of wave with averages FI of images
        String m stdDev wavename dec // name of wave with std dev FI of images
       m avg wavename=imagewavename+" AVG FI"
        m stdDev wavename=imagewavename+" STD FI"
        m avg wavename dec=m avg wavename+" DEC"
       m stdDev wavename dec=m stdDev wavename+" DEC"
       make/d/0/N=(m layers)
$m avg wavename,$m stdDev wavename,$m avg wavename dec,$m stdDev wavename dec
        variable index1=0
        variable m avg FI,m std FI
        do
               // make an image
```

```
m_newwavename = imagewavename+"frame"+ num2str(index1)
               Make/O/N=(m rows, m columns) $m newwavename
                $m newwavename = $imagewavename[p][q][index1]
                // Threshold
                // make px number < Threshold -> Nan
               setnan($m newwavename,m rows,m columns, Thre)
               WaveStats/Q $m newwavename
               m avg FI = V avg
               m std FI = V sdev
               print index1, m_avg_FI,m_std_FI, m_newwavename
                $m avg wavename[index1]=m avg FI
                $m avg wavename dec[index1]=m avg FI
                $m stdDev wavename[index1]=m std FI
                $m stdDev wavename dec[index1]=m std FI
                index1 += 1
        while(index1 < m layers)</pre>
        Resample/DOWN=6 $m avg wavename dec, $m stdDev wavename dec
        display $m avg wavename, $m_avg_wavename_dec
        append $m stdDev wavename, $m stdDev wavename dec
        Legend/C/N=text0/A=MC
EndMacro
function setnan(waves, row, col, Thre)
       wave waves
       variable row, col, Thre
       variable p, q
       for (p=0; p<row; p=p+1)</pre>
               for (q=0;q<col;q=q+1)
                       if (waves[p][q]<Thre)</pre>
                               waves[p][q]=nan
                       endif
               endfor
        endfor
end function
```

Section 8: State 3/ State 4 average intensity plots

In our work, we reproduced the metabolic state manipulation experiment 3 times, and in each experiment, we studied 3 individual mitochondria that happened to be within the field of view with super-resolution microscopy. All of the traces are shown in Fig. S 6 to Fig. S 13 below.



Fig. S 6. Isolated mitochondria respiration test.



Fig. S 7. Isolated mitochondria respiration test.



Fig. S 8. Isolated mitochondria respiration test.



Fig. S 9. Isolated mitochondria respiration test.



Fig. S 10. Isolated mitochondria respiration test.



Fig. S 11. Isolated mitochondria respiration test.



Fig. S 12. Isolated mitochondria respiration test.



Fig. S 13. Isolated mitochondria respiration test.

Section 9: The standard deviation of the TMRE fluorescence intensity

Fig. S 14 below shows the average TMRE intensity, and the standard deviation, of the fluorescent intensity (FI) in the ROI for each frame, and the ratio of the standard deviation to the average, as a function of time, under different metabolic states. The deviation is about 60 % of the

average, indicating significant spatial fluctuations of the membrane potential due to the ultrastructure. Interestingly, this ratio does not change much with metabolic status.



Fig. S 14. Comparison of TMRE AVG and STD intensity, and the Ratio of STD/AVG.

Section 10: 3D projection

Fig. S 15 below shows the 3D projection of one of the TMRE images showing the spatial variation in a different format.



Fig. S 15. 3D representation of FI. Each pixel in XY is 48 nm.

Section 11: Distribution of the dye after the collapse of the membrane potential (other cell lines)

Fig. S 16 to Fig. S 18 below show the distribution of TMRE in isolated mitochondria before and after membrane potential collapse with CCCP. The zero membrane potential images still show structure, indicating that even under zero membrane potential, there is a small amount of TMRE bound to the membrane.





Fig. S 16. TM<u>RE intensity of isolated mitochondria (HEK293) before</u> and ajter treating with CCCF









The response to oligomycin and CCCP presented in the main text for HeLa cells is also observed in 3 other cell lines (see Fig. 9 19 to Fig. S 20 below).





Fig. S 19. TMRE Intensity of isolated mitochondria (MB231) treated with Oligomycin and CCCP.



Fig. S 20. TMRE Intensity of isolated mitochondria (HEK293) treated with Oligomycin and CCCP.

Section 13: Experimental conditions: Yield and statistics

For each figure in the main text, we present a table of how many times that experiment was performed, and under what conditions. This demonstrates in detail the reproducibility of all the key findings of this paper. In particular, this clearly establishes that we are indeed seeing a common phenomenon, and not just an exception. In order to demonstrate that all conclusions drawn in the manuscript not just based on the few selected images shown, we list out the conclusion for each figure shown and the number of times that experimental conclusion was reproducible.

Conclusion for Fig. 1: "Tubular isolated mitochondria are observed which demonstrate regions of high and low cristae density when labeled with structural dyes such as NAO and mitotracker green and voltage variations when labeled with voltage dye TMRE".

In table 1, we list all the experiments on isolated mitochondria. In 26 of the 49 experiments (53%), tubular mitochondria are visible in the field of view, and were studied in more detail than circular mitochondria (discussed in more detail below), which are visible in all experiments. Typically, when tubular mitochondria are visible, they only constitute about 10% of the total # of visible mitochondria (Lee, et al, manuscript in preparation). Of the 26 tubular mitochondria experiments, in 17 of them the cristae were clearly observed (65%). The criteria to observe the cristae is that, upon performing a line profile along the axis of the tubular structure (manually aligned in ImageJ software), the peak/valley ratio exceeded 50% of mean.

Conclusion for Fig. 2B: "Voltage dye TMRE fluorescence and structure dye NAO fluorescence are correlated".

In the 17 experiments in Table 1 that showed cristae structure in tubular mitochondria, 13 of them had both a voltage and structural dye imaged. Of these 13, all of them showed correlation between the F.I. of the voltage dye and structure dye.

Conclusion for Fig. 2E: "mtDNA is anti-localized with TMRE voltage dye".

This experiment was performed 3 times, and all showed this conclusion.

Conclusion for Fig. 2F: "FCCP collapses TMRE intensity, but there is some non-zero intensity even after FCCP has collapsed the membrane voltage".

Table 2 lists these experiments. In all (6/6=100%), this effect was observed. This includes 4 different cell lines, proving it persists independent of cell line used. Additional figures confirming this are shown in Section 11 in supporting information.

<u>Conclusion for Fig. 4A-B-C: "Changes in mitochondrial membrane potential as a function of time and position can be imaged in different metabolic states, created by the addition of substrates and inhibitors of the electron transport chain."</u>

In Fig. 4B, we applied the respiration test to verify the function of mitochondria after isolation. This experiment was done 3 times (N=3) and 3 mitochondria were analyzed for each experiment

(total of 9 mitochondria). Among all the experiments, all 9 mitochondria showed responses to the addition of succinate (= 100%) and the responsive increase in TMRE signal is varies between 11% to 61 %. 6 out of 9 mitochondria showed responses to the addition of ADP (= 67 %) and the responsive decrease in TMRE is varies between 7 % to 29 %. Also see Section 7, 8, and 9 in supporting information for the detail analysis method and results. These are tabulated in Table 3.

As discussed in Section 8 in supporting information, we reproduced the metabolic state manipulation experiment 3 times, and in each experiment, we studied 3 individual mitochondria that happened to be within the field of view with super-resolution microscopy. All of the traces are shown in Fig. S 6 to Fig. S 13

In Fig. 4C, we used oligomycin to verify the mitochondrial function responding to inhibition of ATP synthesis. The experiment was done 4 times (N=4). Among all the experiments, 3 out of 4 times the mitochondria had responded to the addition of oligomycin (= 75% chance to show response to ATP synthesis inhibition) and the responsive increase in TMRE signal is varies between 17% to 52 %. See also Section 12 in supporting information, which shows additional reproducibility of Fig. 4C in two other cell lines, for a total of 3 cells.

Date	Cell used (Passage #)	Microscope	Lables	Record for I	solated Mitochondr	ia with Cri	stae observed (Fig	g 1) Rivel time [us]	Divel Size [nm]	FOV [um]	Seeing Cristae?	Shane
9/1/21	Hela (P15)	Zeiss LSM 900	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (0.3%)	63x	561-700	3 54	49	24 18x24 18	y	circular
0/12/24	(010)	(Airyscan) Zeiss LSM 900	TMRE	100 nM; 15 min; DMEM 10 nM; 15 min; DMEM	λ _{ex} 488nm (0.1%) λ _{ex} 561nm (0.8%)	624	450-561 561-700	53.75	40	F FONE FO	v	tubular
9/12/21	HeLa (P18)	(Airyscan)	MTG	100 nM; 15 min; DMEM	λ _{ex} 488nm (0.5%)	63X	450-561	62.60	49	5.50x5.50	Ŷ	tubular
9/13/21	HeLa (P18)	(Airyscan)	MTG	100 nM; 15 min; DMEM	λex488nm (1.2%)	63x	450-561	8.24	42	6.34x6.34	Y	circular
9/15/21	HeLa (P18)	Zeiss LSM 900 (Airyscan)	TMRE MTG	10 nM; 15 min; DMEM 100 nM; 15 min; DMEM	λ _{ex} 561nm (0.5%) λ _{ex} 488nm (0.5%)	63x	561-700 450-561	8.24	49	6.62x6.62	Y	tubular/ circular
9/20/21	HeLa (P7)	Zeiss LSM 900 (Airyscan)	TMRE	10 nM; 15 min; DMEM 100 nM: 15 min; DMEM	λ _{ex} 561nm (0.7%)	63x	561-700 450-561	16.16	49	11.64x11.64	Y	circular
9/22/21	HeLa (P8)	Zeiss LSM 900	TMRE	10 nM; 15 min; DMEM	λex561nm (0.7%)	63x	561-700	10.49	49	8.26x8.26	Y	tubular
0/24/21	Hota (D9)	(Airyscan) Zeiss LSM 900	TMRE	100 nM; 15 min; DMEM 10 nM; 15 min; DMEM	λex488nm (0.6%) λex561nm (0.2%)	624	450-561 561-700	0.91	49	0.40×0.40	v	circular
9/24/21	HeLa (P8)	(Airyscan) Zeiss I SM 900	MTG TMRF	100 nM; 15 min; DMEM	λ _{ex} 488nm (0.6%)	05X	450-561	9.81	49	9.4039.40	Ŷ	circular
9/27/21	HeLa (P9)	(Airyscan)	MTG	100 nM; 15 min; DMEM	λ _{ex} 488nm (0.2%)	63x	450-561	5.24	42	7.55x7.55	Y	tubular
9/28/21	HeLa (P9)	Zeiss LSM 900 (Airyscan)	TMRE MTG	10 nM; 15 min; DMEM 100 nM; 15 min; DMEM	λex561nm (0.7%) λ _{ex} 488nm (0.7%)	63x	561-700 450-561	7.11	43	11.66x11.66	Y	tubular
10/4/21	HeLa (P10)	Zeiss LSM 900 (Airvscan)	TMRE NAO	10 nM; 15 min; DMEM 100 nM; 15 min; DMEM	λ _{ex} 561nm (0.5%) λ _{ex} 488nm (0.5%)	63x	561-700 450-561	14.21	43	11.66x11.66	N	circular
10/15/21	HeLa (P13)	Zeiss LSM 900	TMRE	10 nM; 15 min; DMEM	λex561nm (0.4%)	63x	561-700	2.61	42	6.34x6.34	N	circular
10/20/21	Hela (P14)	Zeiss LSM 900	TMRE	10 nM: 15 min: DMEM	λ _{ex} 4881111 (0.3%)	63x	561-700	7.83	47	3.19x3.19	Y	circular
10/20/21		(Airyscan) Zeiss LSM 900	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (1.0%)		561-700					
11/5/21	HeLa (P7)	(Airyscan)	MTG	100 nM; 15 min; DMEM	λex488nm (0.5%)	63x	450-561	5.31	42	16.90x16.90	N	circular
11/13/21	HeLa (P8)	(Airyscan)	NAO	100 nM; 15 min; DMEM	λex488nm (1.0%)	63x	450-561	3.92	43	7.43x7.43	Y	circular
11/30/21	HeLa (P10)	Zeiss LSM 900 (Airyscan)	TMRE NAO	10 nM; 15 min; DMEM 100 nM; 15 min; DMEM	λ _{ex} 561nm (5.0%) λ _{ex} 488nm (1.0%)	63x	561-700 450-561	3.92	43	8.45x8.45	Y	tubular/ circular
12/3/21	HeLa (P11)	Zeiss LSM 900 (Airyscan)	TMRE MTG	10 nM; 15 min; DMEM 100 nM: 15 min; DMEM	λ_{ex} 561nm (2.0%) λ_{ex} 488nm (0.2%)	63x	561-700 450-561	3.27	43	10.14x10.14	Y	tubular
1/7/22	HeLa (P9)	Zeiss LSM 900	TMRE	10 nM: 15 min: DMEM	λ _{ex} 561nm (2.0%)	63x	561-700	0.85	46	10.14x10.14	Y	tubular
1/10/22		(Airyscan) Zeiss LSM 900	TMRE	10 nM; 15 min; DMEM	λex561nm (5.0%)	624	561-700	1.21	42	11 66-11 66	N	eireuler
1/10/22	HeLa (P10)	(Airyscan) Zeiss I SM 900	MTG TMRF	100 nM; 15 min; DMEM	λ _{ex} 488nm (4.5%)	03X	450-561	1.51	45	11.00X11.00	IN	circular
1/16/22	HeLa (P11)	(Airyscan)	MTG	100 nM; 15 min; DMEM	λex488nm (0.3%)	63x	450-561	2.22	43	10.14x10.14	Y	circular
2/3/22	HeLa (P13)	Zeiss LSM 900 (Airyscan)	MTG	10 nM; 15 min; DMEM 100 nM; 15 min; DMEM	λ _{ex} 561nm (2.0%) λ _{ex} 488nm (3.0%)	63x	561-700 450-561	1.15	43	76.99x76.99	N	circular
2/4/22	HeLa (P13)	Zeiss LSM 900 (Airvscan)	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (0.5%)	63x	561-700	4.07	49	12.68x12.68	Y	tubular
2/8/22	L6 (P6)	Zeiss LSM 900	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (1.0%)	63x	561-700	3.72	43	10.14x10.14	Y	tubular
2/11/22	Hel a (P16)	Zeiss LSM 900	TMRE	10 nM; 15 min; DMEM 10 nM; 15 min; DMEM	λex488nm (1.0%) λex561nm (1.0%)	63v	561-700	10.66	13	8 44 × 8 44	v	tubular
2/11/22	(10)	(Airyscan) Zeiss LSM 900	MTG TMRE	100 nM; 15 min; DMEM 10 nM; 15 min; DMEM	λ _{ex} 488nm (0.5%) λ _{ex} 561nm (2.0%)		450-561 561-700	20.00	-13			
2/14/22	HeLa (P17)	(Airyscan)	MTG	100 nM; 15 min; DMEM	λ _{ex} 488nm (2.0%)	63X	450-561	3.55	43	12.68X12.68	Ŷ	circular
3/25/22	HeLa (P7)	(Airyscan)	MTG	100 nM; 15 min; DMEM	λex488nm (1.0%)	63x	450-561	4.45	43	10.14x10.14	N	circular
3/30/22	HeLa (P7)	Zeiss LSM 900 (Airyscan)	TMRE MTG	10 nM; 15 min; DMEM 100 nM; 15 min; DMEM	λex561nm (3.0%) λ _{ex} 488nm (1.0%)	63x	561-700 450-561	1.15	43	78.01x78.01	N	circular
4/1/22	HeLa (P7)	Zeiss LSM 900 (Airyscan)	TMRE MTG	10 nM; 15 min; DMEM 100 nM: 15 min; DMEM	λex561nm (2.0%) λex488nm (1.0%)	63x	561-700 450-561	4.45	43	10.14x10.14	Y	circular
4/4/22	HeLa (P8)	Zeiss LSM 900	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (2.0%)	63x	561-700	8.13	41	5.32x5.32	Y	circular
4/8/22	Hela (P9)	Zeiss LSM 900	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (3.0%)	63x	561-700	8 13	41	4 34x4 34	v	circular
1,0,22	11020 (15)	(Airyscan) Zeiss LSM 900	MTG TMRE	100 nM; 15 min; DMEM 10 nM; 15 min; DMEM	λ _{ex} 488nm (3.0%) λex561nm (2.0%)		450-561 561-700	10.20				tubular/
4/13/22	HeLa (P10)	(Airyscan)	MTG	100 nM; 15 min; DMEM	λ _{ex} 488nm (2.0%)	63x	450-561	10.66	43	8.45x8.45	N	circular
4/15/22	HeLa (P10)	(Airyscan)	MTG	100 nM; 15 min; DMEM	λ _{ex} 488nm (4.0%)	63x	450-561	14.21	42	6.43x6.43	Y	circular
4/25/22	HeLa (P12)	Zeiss LSM 900 (Airyscan)	TMRE MTG	10 nM; 15 min; DMEM 100 nM; 15 min; DMEM	λ _{ex} 561nm (1.0%) λ _{ex} 488nm (1.0%)	63x	561-700 450-561	5.22	43	6.34x6.34	Y	tubular/ circular
5/3/22	HeLa-GFP (P8)	Zeiss LSM 900 (Airyscan)	TMRE GEP	10 nM; 15 min; DMEM	λex561nm (4.0%) λex488nm (4.0%)	63x	561-700 450-561	1.79	42	4.06x4.06	Y	tubular
5/3/22	L6 (P8)	Zeiss LSM 900	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (4.0%)	63x	561-700	2.15	42	3.38x3.38	N	tubular/
5/11/22	16 (PQ)	Zeiss LSM 900	TMRE	10 nM; 15 min; DMEM 10 nM; 15 min; DMEM	λ _{ex} 488nm (4.0%) λ _{ex} 561nm (4.0%)	63v	450-561 561-700	23	12	6 34y6 34	v	tubular
5/11/22	20 (19)	(Airyscan) Zeiss LSM 900	PicoGreen TMRE	3 ul/ml; 15 min; DMEM 10 nM: 15 min: DMEM	λ _{ex} 488nm (1.0%) λ _{ex} 561nm (4.0%)	034	450-561 561-700	2.5	42	0.54x0.54		
5/14/22	HeLa (P12)	(Airyscan)	MTG	100 nM; 15 min; DMEM	λ _{ex} 488nm (4.0%)	63x	450-561	2.3	42	6.34x6.34	Ŷ	tubular
5/18/22	HeLa (P13)	(Airyscan)	MTG	100 nM; 15 min; DMEM	λ _{ex} 488nm (4.0%)	63x	450-561	2.3	42	6.34x6.34	Y	circular
6/6/22	HeLa (P15)	STED Zeiss LSM 900	TMRE TMRE	10 nM; 15 min; DMEM 10 nM; 15 min; DMEM	λ _{ex} 561nm (10%) λ _{ex} 561nm (1.0%)	100x	561-700 561-700	10	18	4.00x5.00	N	circular
6/13/22	HeLa (P16)	(Airyscan) Zeiss I SM 900	MTG	100 nM; 15 min; DMEM	λex488nm (4.0%)	63X	450-561	1.43	43	5.07x5.07	Ŷ	tubular/
6/20/22	HeLa (P18)	(Airyscan)	MTDR	10 nM; 15 min; DMEM	λ _{ex} 641nm (4.0%)	63x	642-700	1.5	56	5.00x5.00	Y	circular
6/21/22	HeLa (P19)	Zeiss LSM 900 (Airyscan)	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (4.0%)	63x	561-700	1.32	49	12.68x12.68	Y	tubular/ circular
6/23/22	HeLa (P19)	Zeiss LSM 900 (Airyscan)	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (5.0%)	63x	561-700	0.84	49	24.18x24.18	Y	circular
6/28/22	HeLa (P20)	Zeiss LSM 900	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (2.0%)	63x	561-700	2.65	49	39.00x39.00	Y	circular
7/18/22	Hela (P23)	Zeiss LSM 900	TMRF	10 nM: 15 min: DMEM	λ _m 561nm (5.0%)	63x	561-700	1.32	49	78.01x78.01	N	circular
42/07/22	1000 (120)	(Airyscan) Zeiss LSM 900	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (0.8%)		561-700	2.52		2 54 5 45		en cultar
12/17/22	MB231 (P9)	(Airyscan)	MTG	100 nM; 15 min; DMEM	λex488nm (2.0%)	63x	450-561	2	49	3.54x5.45	Ŷ	tubular
12/17/22	HEK293 (P5)	(Airyscan)	MTG	100 nM; 15 min; DMEM	λex488nm (2.0%)	63x	450-561	1.44	49	3.24x3.28	Y	circular
12/26/22	HEK293 (P6)	Zeiss LSM 900 (Airyscan)	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (1.0%)	63x	561-700 450-561	1.32	49	11.5x11.5	Y	tubular
12/27/22	HEK293 (P6)	Zeiss LSM 900 (Airyscan)	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (2.0%)	63x	561-700 450-561	0.97	49	6.99x6.70	Y	tubular
12/28/22	HK2 (P3)	Zeiss LSM 900	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (1.0%)	63x	561-700	0.97	49	37.83x37.83	Y	tubular
		(Airyscan)					400-501	L	L			

Table 1. Record and statistic table for Fig. 1. Within a total of 49 isolated mitochondria experiments, 38 of them shows cristae structure in isolated mitochondria with TMRE dye (78 %), and 26 of them sustained in tubular shape (53 %). Within a total of 26

tubular shape isolated mitochondria experiments, 17 of them were able to show cristae morphology through line profiling (65 %).

	Record for Isolated Mitochondria Treat with CCCP (Fig 2F)											
Date	Cell used (Passage #)	Microscope	Lables	Staining condition	Laser settings	Objective	Detection (nm)	Pixel time [µs]	Pixel Size [nm]	FOV [µm]	Seeing Cristae?	Shape
5/11/22	L6 (P9)	Zeiss LSM 900 (Airyscan)	TMRE MTG	10 nM; 15 min; DMEM 100 nM; 15 min; DMEM	λ _{ex} 561nm (4.0%) λ _{ex} 488nm (1.0%)	63x	561-700 450-561	2.3	42	6.34x6.34	Y	tubular
12/26/22	MB231(P11)	Zeiss LSM 900 (Airyscan)	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (4.0%)	63x	561-700	0.85	49	16.90x16.90	Y	tubular
12/26/22	HEK293 (P6)	Zeiss LSM 900 (Airyscan)	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (1.0%)	63x	561-700	1.32	49	11.5x11.5	Y	tubular
12/27/22	HEK293 (P6)	Zeiss LSM 900 (Airyscan)	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (2.0%)	63x	561-700	0.97	49	3.52x3.47	Y	tubular circular
12/28/22	HK2 (P3)	Zeiss LSM 900 (Airyscan)	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (1.0%)	63x	561-700	0.97	49	39.00x39.00	Y	tubular
12/28/22	HK2 (P3)	Zeiss LSM 900 (Airyscan)	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (2.0%)	63x	561-700	0.84	49	2.98x2.93	Y	tubular

Table 2. Record and statistic table for Fig. 3. We've examined the line profile of isolated mitochondria before and after treatment with CCCP (N=6, with 4 different kinds of cell lines).

	Record for Isolated Mitochondria Respiration Experiment (Fig 4A)											
Date	Cell used (Passage #)	Lables	Laser settings	Detection (nm)	Pixel time [µs]	Pixel Size [nm]	FOV [µm]	Shape	Percentage increase due to succinate	Two Drops by ADP addition	Percentage of 1 st drop	Percentage of 2 nd drop
06/21/22 mito1	HeLa (P19)	TMRE	λ _{ex} 561nm (4.0%)	561-700	1.32	49	12.68x12.68	tubular/ circular	11%	Y	17%	21%
6/21/22 mito2	HeLa (P19)	TMRE	λ _{ex} 561nm (4.0%)	561-700	1.32	49	12.68x12.68	tubular/ circular	24%	Y	8%	7%
6/21/22 mito3	HeLa (P19)	TMRE	λ _{ex} 561nm (4.0%)	561-700	1.32	49	12.68x12.68	tubular/ circular	16%	Y	13%	11%
6/23/22 mito1	HeLa (P19)	TMRE	λ _{ex} 561nm (5.0%)	561-700	0.84	49	24.18x24.18	circular	46%	Y	29%	19%
6/23/22 mito2	HeLa (P19)	TMRE	λ _{ex} 561nm (5.0%)	561-700	0.84	49	24.18x24.18	circular	39%	N	N/A	N/A
6/23/22 mito3	HeLa (P19)	TMRE	λ _{ex} 561nm (5.0%)	561-700	0.84	49	24.18x24.18	circular	61%	N	N/A	N/A
6/28/22 mito1	HeLa (P20)	TMRE	λ _{ex} 561nm (2.0%)	561-700	2.65	49	39.00x39.00	circular	16%	Y	20%	19%
6/28/22 mito2	HeLa (P20)	TMRE	λ _{ex} 561nm (2.0%)	561-700	2.65	49	39.00x39.00	circular	21%	N	N/A	N/A
6/28/22 mito3	HeLa (P20)	TMRE	λ _{ex} 561nm (2.0%)	561-700	2.65	49	39.00x39.00	circular	15%	Y	13%	11%

Table 3. Record and statistic table for Fig. 4A. The rate of mitochondria showing response to ADP addition is 67 %. The percentage drop of TMRE intensity varies between mitochondria from 7 % to 29 % (N=3).

	Record for Isolated Mitochondria Treat with Oligomycin (Fig 4C)										
Date	Cell used (Passage #)	Microscope	Lables	Staining condition	Laser settings	Detection (nm)	Pixel time [µs]	Pixel Size [nm]	FOV [µm]	Response to Oligomycin	Percentage of Change
5/11/22	L6 (P9)	Zeiss LSM 900 (Airyscan)	TMRE MTG	10 nM; 15 min; DMEM 100 nM; 15 min; DMEM	λ _{ex} 561nm (4.0%) λ _{ex} 488nm (1.0%)	561-700 450-561	2.3	42	6.34x6.34	Y	52%
12/26/22	MB231(P11)	Zeiss LSM 900 (Airyscan)	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (4.0%)	561-700	0.85	49	16.90x16.90	N	N/A
12/27/22	HEK293 (P6)	Zeiss LSM 900 (Airyscan)	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (2.0%)	561-700	0.97	49	3.52x3.47	Y	17%
12/28/22	HK2 (P3)	Zeiss LSM 900 (Airyscan)	TMRE	10 nM; 15 min; DMEM	λ _{ex} 561nm (1.0%)	561-700	0.97	49	39.00x39.00	Y	24%

Table 4. Record and statistic table for Fig. 4C. The rate of mitochondria showing response to Oligomycin addition is 75%. The percentage change of TMRE intensity varies between mitochondria from 17 % to 52 % (N=4).

	Record for Seahorse Experiment									
Date	Cell used (Passage #)	Instrument	Chemical Addition	Response to ADP	Response to Oligomycin	Response to CCCP	Response to Rotenone	Respiratory Control Ratio (RCR)		
10/17/19	HeLa cell (P12)	Seahorse XFe24	55 μL, 40 mM ADP; 60 μL, 25 μg/mL oligomycin, 65 μL, 40 μM FCCP;	Y	Y	Y	N/A	2.37		
1/5/22	Mouse Heart	Seahorse XFe24	55 μL, 40 mM ADP; 60 μL, 25 μg/mL oligomycin, 65 μL, 40 μM FCCP; 70 μL, 40 μM Rotenone	Y	Y	У	Y	3.9		

Table 5. Record and statistic table for the Seahorse experiment. We've done the respiration test on both isolated mitochondria from HeLa cells and the mouse heart. The Respiratory Control Ratio (RCR) was 2.37 and 3.9, respectively (N=1).

	Record for Isolated Mitochondria with STED										
Date	Cell used (Passage #)	Lables	Staining condition	Laser settings	Objective	Detection	Pixel time	Pixel Size [nm]	FOV [µm]	Seeing Cristae?	Shape
			•	-		(nm)	[µs]			-	
6/6/22	Hola (P15)	TMPE	10 nM; 15 min;	3 561 nm (10%)	100v	561-700	10	19	4 00 ×5 00	N	circular
0/0/22	field (F13)	TIVINE	DMEM	Aex 3011111 (1076)	1007	501-700	10	10	4.00x3.00	IN	circular
6/6/22 HeLa		(P15) MTDR ¹⁰	10 nM; 15 min;	λ _{ex} 641nm	100x	642-700	10	15	34.00x34.0	Y c	aireular
	песа (Р15)		DMEM	(4.0%)					0		circular

Table 6. Record and statistic table for isolated mitochondria observed by STED microscope. We were able to resolve mitochondria cristae with MTDR but not TMRE (N=1).

Section 14: Relationship to Murphy et al ¹⁶

In the main text, we have clarified that, even under zero potential, there is still TMRE bound to the membrane. One could in principle call the binding to the outer membrane (buffer or cytosol side) potential independent binding. Only the TMRE bound to the inner membrane (matrix side) is potential dependent, since the free TMRE in the matrix is potential dependent, and the amount bound on the matrix side is proportional to the free TMRE in the matrix. We have also referenced key previous literature that deals with this.

Murphy studied "potential independent binding" extensively, for example, ref ¹⁶. His cartoon (Fig. 1A) is identical to our cartoon (Fig. 3A), in principle, which again is equivalent to Rottenberg 1984 which we cited in our original draft manuscript. In Murphy's work, he studied the "proportion of cation that is membrane bound" for different TPP⁺ conjugates. The conjugates of various linker lengths, up to 15 carbon atoms, became gradually more hydrophobic as the linker length increased. Therefore, he found, the "proportion of cation that is membrane bound" became gradually larger and larger as the linker length was increased by his lab and students.

The relationship to our model presented In Fig. 3 in the main text is as follows: Murphy essentially studied the constant "a_i", which in our model is the binding coefficient between the bound and free TMRE in the matrix. Murphy called this the "proportion of cation that is membrane bound" in the matrix. Murphy found, logically, that the more hydrophobic the moiety was, the larger the value of a_i , i.e. the larger the fraction bound to the membrane. In our work, we used TMRE which has a known and measured value of a_i from the literature, measured by many groups for TMRE. Whereas, Murphy measured that binding coefficient for other species of lipophilic cations that, while related in structure to the TMRE used in this work, are chemically different. Therefore, Murphy's binding coefficient measurements in ref ¹⁶ are not directly applicable to our work. The way the value of a_i was measured for TMRE by other groups is discussed in detail in Section 3 in supporting information above.

Note, for Murphy, a_o also increased with the hydrophobicity of his compounds, so that his compounds also bound to the outer membrane with increasing binding coefficient as a function of

hydrophobicity, to the point where in extreme cases, he observed significant "uptake" even with no membrane voltage.

However, it is important to note that, no matter what value of binding coefficient (a_i, a_o) , there is ALWAYS some membrane binding. It is just not measurable in all "uptake" experiments if the voltage is zero and (a_i, a_o) are small. This is why we initially did not notice it in our super-resolution experiments, until we re-examined the images and, lo and behold, even at zero voltage (CCCP collapsed), we were able to image the bound TMRE and show it had structure related to the cristae and mitochondrial internal ultrastructure (Fig. 2F).

Section 15: Biological Implications: Disease and health in mitochondria.

The internal ultra-structure of mitochondria has long and recently been known to be important in health and disease, including stem cell biology ¹⁷, cancer ¹⁸, and aging ¹⁹. Our work extends the ultrastructure studies to functional studies, allowing the superresolution electrophysiology of mitochondria to be directly tested in response to pharmacological manipulation of metabolism for future studies in aging, disease, and health. Summarizing: "*Novel research on the functional relevance of compartmentalization has highlighted a key role of regulated cristae subcompartment structure in bioenergetics and in human diseases.*" ²⁰

The topic of mitochondria ultrastructure has been studied with TEM and on fixed cells extensively because of new findings about the relevance to apoptosis and metabolism ^{21–26}. It is not just the ultrastructure: the membrane potential (bioelectronic property) also plays a critical role in the physiology of the organelle & cell: "*Cristae dynamics and local changes in mitochondrial membrane potential at the level of individual cristae are predicted to have major consequences for mitochondrial functions such as oxidative phosphorylation, thermogenesis,* Ca2⁺ homeostasis, and apoptosis." ²⁷

Outstanding questions that the methods and techniques presented in this work can help to address in future studies are: What are the energy requirements of cristae membrane dynamics? ²⁷ Do other molecular players regulate cristae membrane dynamics? ²⁷ How are cristae dynamics affected during apoptosis? ²⁷ How do cristae dynamics affect the superresolution organization of redox nanodomains and redox signaling? ²⁷ What is the role of cristae architecture in mitochondrial bioenergetics? ²⁰

For example, what might be the difference between interfibrillar and subsarcolemmal mitochondria in muscle cells? What is the functional difference between cerebellar Purkinje vs. granular cell mitochondria? In a cell harboring a heteroplasmic mitochondrial DNA disease mutation, are the mitochondria physiologically different depending on their resident mitochondrial DNA genotype or are all of the mitochondria functionally similar due to homogenization by fusion and fission? Are mitochondria undergoing mitophagy (a membrane potential dependent phenomenon) physiologically different from the mitochondria that will be retained?

Note that this manipulation of metabolic states in state 3 and state 4 is not possible in whole cells, and so this clearly demonstrates a significant advance above the already significant live cell imaging of TMRE in whole cells in ref. ²⁸.

Section 16: Spatial and temporal statistical properties and mitochondrial heterogeneity

Prior to this work (and the advent of super-resolution microscopy), researchers were only able to experimentally measure the total amount of TMRE taken up by mitochondria, without resolving where within the organelle it was located. In practice, the entire organelle would appear as one voxel/pixel, and the intensity so measured of the voxel was the average fluorescence intensity, and hence, proportional to the average TMRE density inside the mitochondria. This work shows for the first time the evolution of the electrophysiology at the superresolution scale as the mitochondria translate between different metabolic states.

Mitochondrial DNA exhibits heterogeneity from one organelle to the next, even within a single cell, a phenomenon termed heteroplasmy: Each individual mitochondria carries a different DNA copy 29,30 . Therefore, functional differences between mitochondria are to be expected. We term this "functional heterogeneity". In orthogonal measurements under identical conditions, we performed TPP⁺ analysis of the membrane potential 31,32 . If we compare the effect of succinate to the membrane potential change, the result from the TPP⁺ test (calculated ~ 27 % increase) is comparable to our data in this manuscript (11 % – 24 %). Although our studies of single mitochondria are consistent with the ensemble membrane potential studies using TPP⁺ electrodes 31 , it should be expected that there is some spread in the membrane potential of one mitochondrion to the next, discussed next.

In our work, we reproduced the metabolic state manipulation experiment 3 times, and in each experiment, we studied 3 individual mitochondria that happened to be within the field of view with super-resolution microscopy. With this sample size of 9, we found 66 % of the mitochondria demonstrated a change in average membrane potential upon state 3/state 4 transitions. The change was between 5 % -20 %. The overall average membrane potential of each mitochondrion varied from one mitochondrion to the next. Although 9 is a small sample size, this is a demonstration of functional heterogeneity plasmy in isolated mitochondria. Although beyond the scope of this paper, scaling this to 96 well plates or even microfluidic chambers could enable massively parallel interrogation of mitochondrial functional heteroplasmy.

Our measurements also enable quantitative measurement of both the spatial and temporal variation of the membrane potential within a single, individual mitochondrion. The spatial variation of the mitochondrial membrane potential was calculated as the ratio of the standard deviation of the fluorescent intensity (FI) inside the ROI divided by the average FI inside the ROI. The ROI is the mitochondria (see SI). During the metabolic manipulation, we found the variation to be about 60 % of the average FI and did not change significantly during the transition from state 3 to state 4 (Fig. S 14). As for the temporal variation, we calculated the average intensity at each interrogation point and this shows some variation of order 10 % of the total fluorescence intensity (hence potential) as a function of time. While this could be partially from instrumental noise, this is an upper limit on fluctuation on the second timescale of the average mitochondrial membrane potential. This is the first proof of concept use of super-resolution microscopy to determine spatial and temporal fluctuations of the mitochondrial membrane potential along a single, isolated mitochondrion. Clearly, improvements in the spatial and temporal resolution will be an intriguing avenue for future research, enabling potentially for the first time to ask the question of whether there is a Hogdkins-Huxley equivalent model (which we would term the Burke-Wallace model) of mitochondrial membrane dynamics ³³.

Section 17: Resolution discussion

It is absolutely true we cannot resolve which side of the inner membrane the TMRE is localized to with the given setup. In fact, to resolve that, one would need to resolve with better resolution than the size of the lipid bilayer (~ 4 nm), which is beyond the capability of any live cell microscopy technique.

However, experiments over 40 years on liposomes have shown lipophilic cations (such as TMRE) are taken INTO the liposome in a voltage dependent manner. Furthermore, they have shown by spin EPR studies and other studies that after it is taken up, it binds to the inside of the liposome membrane^{34–36}. Furthermore, many experiments over the last 40 years^{2–4,31,32,34–41} have shown that lipophilic cations such as TMRE are taken up by mitochondria INTO the matrix when it is fed substrates and inhibitors of the electron transport chain, and that it is released back into the buffer/cytosol when the membrane potential is shorted to zero with FCCP. So, there is plenty of evidence that TMRE is taken up INTO the mitochondria matrix in response to a membrane potential. Nobody doubts this, and nobody has any reason to doubt it, even though they cannot see it. Our results confirm this finding that has been repeated thousands of times around the world. There is also an excellent model based on the Nernst equation that supports this ^{2–4,31,32,34–41}. Therefore, our work is the first to show experimentally in vital isolated mitochondria that the TMRE is localized near the cristae, and the models to date showed indirectly that they are localized on the inside, not outside, i.e. matrix side of the inner membrane.

Notice that voltage drop is across the inner membrane, which is folded (see Fig. 1A). The outer membrane is completely porous to small and even medium sized molecules.

Furthermore, the outer membrane is sometimes parallel to the inner membrane (see Fig. 1), and the space between them (called the "intermembrane space") is typically less than 20 nm. So in some images where the outer membrane is seen (e.g. Fig. S1B), it is typically so close to the parallel inner membrane that both are imaged within the resolution of the microscope.

Section 18: Comparison between Airyscan, STED, and Lattice SIM microscopy

Airyscan and STED were described and investigated for voltage imaging above. In this section, we provide data from Lattice SIM (Structured Illumination Microscopy) for voltage imaging with TMRE.

In Lattice SIM, the sample area is illuminated with a lattice spot pattern instead of grid lines as in conventional SIM. This leads to a higher imaging speed, higher contrast, and less bleaching of fluorophores, which makes it suitable for time-series studies in bio samples ⁴². Noted that Lattice SIM microscopy can achieve imaging at fast frame rates, typically ranging from several frames per second to several tens of frames per second, depending on the resolution and the sample. In principle, Lattice SIM with SIM² processing can provide with a resolution of down to 60 nm. However, with preliminary experiments, when using TMRE (Elyra 7 Lattice SIM with SIM² processing), we found a resolution of around 200 nm (using the FWHM of a line profile of the smallest observable feature in Fig. S 21), much worse than STED or Airyscan for voltage imaging. Therefore, we did not pursue this imaging method.



Fig. S 21. Lattice SIM image of mitochondria in HeLa cells stained with mitotracker green (blue) and TMRE (purple)

Section 19: Wide view of isolated mitochondria: "Zoom out" vs. "Zoom in"

We are limited to about an hour of imaging since the mitochondria die about an hour after isolation. In addition, when we "zoom out" (e.g. 6-10x larger field of view), we are limited in resolution and cannot resolve internal microstructure. Therefore, instead of doing many "zoom" images on one sample, we were forced to do many individual experiments over the course of 2 years to build up meaningful statistics, as shown in Section 13 in supporting information. This does not change the findings of the paper.



Fig. S 22. The wide-view image for Fig. 2B in the manuscript.



Fig. S 23. Wide-view image for Fig. 2E in the manuscript.

In this paper, we present mostly the "zoom in" images to show the inner structure of isolated mitochondria. Here we explained the reason for presenting the "zoom in" images in this draft, and present "zoom out" images for each "zoom in" image presented in the paper.

Fig. S 22 and Fig. S 23 show zoom out of mitochondria presented as zoom in in Fig. 2. Clearly, the mitochondria cristae are reproducible and the conclusions sound when zoomed out. However, these were in whole cells, where no circular mitochondria were observed when the cells were properly treated.

For isolated mitochondria, Fig. S 24 and Fig. S 25 represent typical "zoom out" images. First, we notice, as discussed above, that the number of circular mitochondria out numbers the number of tubular mitochondria. In the interest of time for this paper, we focused on the tubular mitochondria. The circulate mitochondria will be studied in a different manuscript (Lee, et al, manuscript in preparation), and are beyond the scope of this work.

Second, the internal ultrastructure of the mitochondria is difficult to resolve in the "zoom out" images. Furthermore, generating zoom out images take 10x longer (~5 seconds for each laser channel) than zoom in images (<400 ms for each laser channel), during which time motion blurring may be more significant (see "Protocols for visualization of mitochondria structure using Airyscan and STED microscopy" in the materials and methods section of the main manuscript). Therefore, instead of doing many "zoom" images on one sample, we were forced to do many individual experiments over the course of 2 years to build up meaningful statistics, as shown in the Section 13 in supporting information.



Fig. S 24. Wide-view images of isolated mitochondria stained with TMRE (orange) and MTG (green). This is the same data as Fig. 4A in the manuscript. ROI (zoom region) indicated was presented in the main text.



Fig. S 25. Wide-view images for 4C in the manuscript. ROI (zoom region) indicated was presented in the main text.

Year	Author	Microscope	Image Resolution	Dye used	Structure/ Function	In cell/ Isolated	Publication
2019	Dane. W.	Airyscan	150 nm	MTG/TMRE	Structure/Voltage	In cell	Individual cristae within the same mitochondrion display different membrane potentials and are functionally independent
2019	Till. S.	STED	74 nm	SNAP-tag	Structure	In cell	Live-Cell STED Nanoscopy of Mitochondrial Cristae
2019	Chenguang. W.	STED	45 nm	MitoPB Yellow	Structure	in cell	A photostable fluorescent marker for the superresolution live imaging of the dynamic structure of the mitochondrial cristae
2020	Xusan. Y.	STED	35.2 nm	MitoESq-635	Structure	In cell	Mitochondrial dynamics quantitatively revealed by STED nanoscopy with an enhanced squaraine variant probe
2020	Yifang. S.	STED	80 nm	Sirmo	Structure	In cell	Improving Brightness and Stability of Si-Rhodamine for Super-Resolution Imaging of Mitochondria in Living Cells
2022	Tianyan. L	STED	50 nm	РКМО	Structure	In cell	Multi-color live-cell STED nanoscopy of mitochondria with a gentle inner membrane stain
	Ours	Airyscan	120 nm	MTG/NAO/TMRE	Voltage/Respiration	Isolated	

Section 20: Literature review for super-resolution live-cell imaging of mitochondria

Table 7. Literature reviews of mitochondria studies using super-resolution techniques. All The literatures studied structures of mitochondria in cells. We're the only one studied isolated mitochondria and its functions.

The following Table 7 (from refs. ^{28, 10–13}, & ref. ⁴³, which came out while this paper was under review) listed with the name of the publication, type of super-resolution microscope use, image resolution, type of dye use, structural or functional imaging, and in cell or isolated of the recent research related to super-resolution study on mitochondria in live-cells.

Note first that all but one of these measure structure, not voltage. Therefore, "nanoscopy", i.e. sub-50 nm imaging of voltage is still not achieved anywhere in the literature.

Second, the images we have of TMRE with STED, although it is able to image structure very well (80 nm, Fig. S 1, comparable to the literature on live-cells with STED), we found that voltage imaging with STED was still limited to 140 nm.

Third, and finally, none of the work above uses isolated mitochondria. Isolated mitochondria provide advantages above whole cells in manipulating the metabolic state, as discussed in the introduction section of the main text.

A recent review also covers live-cell nanoscopy⁴⁴.

Chemical structure of fluorescent dyes used in this manuscript Section 21:

Nonyl Acridine Orange (NAO)	Tetramethylrhodamine ethyl ester, perchlorate (TMRE)	MitoTracker Green FM (MTG)
• $\lambda_{Ex}/\lambda_{Em}$ = 495/522 nm •Orange solid soluble in DMSO or DMF • C ₂₆ H ₃₈ BrN ₃ •MW: 473	• $\lambda_{Ex}/\lambda_{Em}$ = 549/574 nm •Red solid soluble in DMSO, DMF or EtOH •C ₂₆ H ₂₇ ClN ₂ O ₇ •MW: 515	• $\lambda_{Ex}/\lambda_{Em}$ = 490/516 nm •Orange solid soluble in DMSO • $C_{34}H_{28}CI_5N_3O$ •MW: 672
Me ₂ N N+ (CH ₂)8 CH ₃ Br	Me ₂ N CIO4 CIO4	

Figure references:

https://biotium.com/product/nonyl-acridine-orange-nao/ https://biotium.com/product/tetramethylrhodamine-ethyl-ester-perchlorate-tmre/ https://www.medchemexpress.com/mitotracker-green-fm.html

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Section 22: Confusion on the binding abounds in the literature:

Even as recent as 2018, ref. ⁴⁵ shows a misleading picture of the lipophilic cation TPP⁺ is free and ignores membrane binding in the schematic and in the analysis.



Fig. S 26. Schematic representation of TPP⁺ distribution across the mitochondrial membrane, according to the Nernst equation from.⁴⁵ This example shows how in the literature, membrane binding of lipophylic cations is typically (and incorrectly) ignored. Reprinted from Methods Mol Biol, 1782, Teodoro, J. S.; Palmeira, C. M.; Rolo, A. P., Mitochondrial Membrane Potential ($\Delta\Psi$) Fluctuations Associated with the Metabolic States of Mitochondria, Pages 109–119., Copyright (2018). with permission from Springer Nature.

For ref. ²⁸ work on super-resolution, they have misinterpreted the TMRE fluorescence images:

Quote #1 (from published review/response letter ref.²⁸):

...our data quantifying just the signal from the **diffusible** fraction of TMRE (non-binding and thus sensitive to $\Delta \Psi m$) which also responds differently in the cristae and IBM to oligomycin and FCCP, strongly supports that increased **diffusible** TMRE FI in the cristae is caused by increased $\Delta \Psi m$, when compared to the IBM.

The FIs of the probes at different subcellular compartments can be used to extrapolate the differences in **concentrations** of the probe, which are needed to calculate the difference in $\Delta \Psi m$ between compartments (Ehrenberg et al., 1988; Farkas et al., 1989; Loew et al., 1993; Twig et al., 2008; Wikstrom et al., 2007)."

https://www.embopress.org/action/downloadSupplement?doi=10.15252/embj.2018101056&file= embj2018101056.reviewer_comments.pdf

Comment:

This ignores the bound TMRE, which creates the brightest fluorescence intensity, which we showed in this manuscript. Words like diffusible and concentration refer to free, unbound TMRE which is not what is seen in the images since it is much dimmer than the bound TMRE.

Quotes #2,3 (From supplemental info 46 , 47 , referenced in ref. 28):

The non $\Delta \Psi$ -dependent component of TMRE, also known as the **binding component**, can be **ignored** when calculating relative changes in $\Delta \Psi$ as it is fixed and voltage-independent (2). (2=O'Reilly)

The non- $\Delta \psi$ m-dependent component of TMRE, also known as **the binding component**, can be **ignored** as it is fixed and voltage-independent (Loew et al., 1993;O'Reilly et al., 2003).

Response:

This ignores the bound TMRE on the matrix side to calculate the membrane potential, which creates the brightest fluorescence intensity, which we showed in this manuscript. It was stated in O'Reilly ³⁸ that this needs to be taken into account, but this was not properly applied in ref. ²⁸'s work:

(O'Reilly et al., 2003 ³⁸): TMRE, even at low concentrations, exhibits significant binding to the mitochondrial membrane as found by Scaduto and Grotyohann (1999).

(O'Reilly et al., 2003³⁸): Scaduto and Grotyohann (1999) have shown that TMRE and similar dyes exhibit significant binding to the inner mitochondrial membranes so that most fluorescence comes not from free TMRE but from bound TMRE. (See eq. 1, 2 in that reference, repeated here):

TMRE, even at low concentrations, exhibits significant binding to the mitochondrial membrane as found by Scaduto and Grotyohann (1999). Hence the absolute value for $\Delta \Psi_m$ cannot be determined by a simple Nernstian relationship between [TMRE]_m and [TMRE]_c, but changes in $\Delta \Psi_m$ (flicker amplitude) can be determined from changes in FI as follows. The FI in a mitochondrion is a measure of its total TMRE content, as given by

$$\{\text{TMRE}\}_{\text{total}} = K_{\text{i}}[\text{TMRE}]_{\text{m}} + volume_{\text{m}}[\text{TMRE}]_{\text{m}} + K_{\text{o}}[\text{TMRE}]_{\text{c}} + volume_{\text{im}}[\text{TMRE}]_{\text{c}}, \quad (1)$$

where $\{TMRE\}_{total} = total$ mitochondrial TMRE in units of mass, and $[TMRE]_{c}$ was always 2.5 nM and includes [TMRE] in the mitochondrial intermembrane space.

The following are given in units of volume:

 $volume_{m} = mitochondrial matrix volume$ $volume_{im} = volume of the intermembrane space$ $K_{i} = partition coefficient for [TMRE]_{m}$ binding to the inner mitochondrial membrane

 K_{o} = partition coefficient for [TMRE]_c binding to the inner mitochondrial membrane

 $[\text{TMRE}]_c$ is >300-fold less than $[\text{TMRE}]_m$ in a mitochondrion with $\Delta \Psi_m = -150 \text{ mV}$; *volume*_m and *volume*_{im} are small compared to K_o or K_i ; the value of K_o is 129, and that of K_i is 60 at 28°C (Scaduto and Grotyohann, 1999). (This value for K_i is in precise agreement with the bound:free ratio of 63:1 which we obtained as outlined in the previous paragraph.) Hence, the above expression simplifies to

$$\{\text{TMRE}\}_{\text{total}} = (K_{i} + volume_{m})[\text{TMRE}]_{m}.$$
 (2)

Fig. S 27. Reprinted from Biophysical Journal, 85(5), O'Reilly, C. M., Fogarty, K. E., Drummond, R. M., Tuft, R. A., & Walsh, J. v., Quantitative analysis of spontaneous mitochondrial depolarizations, Pages 3350–3357., Copyright (2003). with permission from Elsevier.³⁸

In this work, we also reference Scaduto 2009³ as a key reference for our interpretation, which explains why the cristae TMRE fluorescence shines bright, whereas inside the matrix the TMRE fluorescence is close to zero.

In summary, Scatudo 2009³, OReilly 2003³⁸, and our paper all clearly state that the TMRE bound to the inside is the dominant amount of TMRE, and is voltage-dependent. Ref. ²⁸ does not correctly interpret this model, and ignores the bound component, only discussing the "diffusible" component, i.e. unbound TMRE.

However, going beyond Scatudo and OReilly, our work is the first to observe the bound component using super-resolution and correctly interpret it.

Section 23: Alternative methods to determine concentrations of dye inside and outside the mitochondria

In this paper, the lipophilic cationic dye concentrations inside and outside the mitochondria are indirectly measured via the fluorescence intensity when quantifying the voltage using the Nernst equation. In principle, this method could be problematic due to the presence of solvent sensitivity: The environment inside and outside mitochondria is different, which could affect the brightness of dyes. One might ask, is there a better way to determine the concentration of dyes inside and outside the mitochondria?

The answer is yes, absolutely, there is a better way to determine the concentration of dyes inside and outside the mitochondria. The better way consists of using an electrochemical sensor of the lipophilic cation that is specific: When the mitochondria take up or release the cation, the external (buffer) concentration can be read out. Since it is read out only in the buffer, there are no artifacts related to the different chemical environments. One only needs to carefully calibrate the system. In fact, this is commonly done in the literature, by many groups, including our own ^{2,31,32}.

In all of the findings in the literature, the results from the external electrochemical electrode are consistent with the fluorescent dye experiments. Therefore, although the artifact that the reader might be concerned with, while in principle a completely legitimate concern, in practice has been shown not to be an issue.

Section 24: Relationship to Miller et al ⁴⁸

As we mentioned in the paper, TMRE is a "tried and true" dye that has been extensively used for over 20 years without artifacts by the mitochondria community. That said, it is always a good idea to investigate new dyes that are faster, more sensitive, etc. Since this is not a review paper, we did not cover all possible voltage dyes.

One new dye approach was published by Miller, et al ⁴⁸. In that work, the technique to probe $\Delta\Psi$ m has been reported that utilizes photoinduced electron transfer (PeT)-based Rhodamine Voltage Reporter (RhoVR) instead of the traditional lipophilic dyes that accumulate in the mitochondria in a $\Delta\Psi$ m-dependent manner ⁴⁸. In principle, such a technique could provide a faster voltage sensor, something that would be very exciting in the context of mitochondrial membrane potential fluctuations discussed in this manuscript. The issue of whether that dye would function in a super-resolution system has yet to be addressed. In addition, the low intensity and high pump powers needed would have to be addressed in the context of mitochondria. Miller et al also observed significant photobleaching, something we are also investigating actively (Burke, et al, manuscript in preparation).

We view this paper as the first step on a journey to dissect the electrophysiology of mitochondria on the nanoscale, not the final step. New dyes and new super-resolution imaging technologies are sorely needed. Ours is the first demonstrated quantitative super-resolution imaging of voltages in mitochondria, but we expect the field to explode now that we have laid the groundwork.

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